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Quantitative Measurement of Aerosol Deposition on Skin, Hair and Clothing for Dosimetric Assessment

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Abstract The deposition to human body surfaces of potentially hazardous aerosol has been investigated through tracer experiments. Particles of different sizes labelled with neutron activatable rare earth tracers were released in test rooms and deposited on volunteers. Various sampling techniques to examine the clearance and retention of the aerosol to skin, hair and clothing were investigated, and a protocol for the most efficient procedure was established and validated. Experiments indicate that the deposition velocity to skin increases linearly with the particle size. A wind tunnel experiment simulating outdoor conditions showed outdoor deposition velocities to be almost an order of magnitude higher than those recorded indoors. Both *in vivo* and *in vitro* experiments were conducted, and the influence of various factors, such as surface type, air flow, heating and electrostatics were examined. The dynamics of particle removal from human skin were studied by fluorescence scanning. Using the experimentally determined parameters, a model was established for calculation of radiation doses received from deposition of airborne radioactive aerosol on human body surfaces. It was found that the gamma doses that could be expected from deposition on skin were of the same order of magnitude as the gamma doses received over several years from contamination on outdoor surfaces. Assuming very high dry contamination levels, as were recorded in some areas of Russia after the Chernobyl accident, it was found that beta doses from skin deposition may amount to several Sievert and thus be responsible for a significant cancer risk.

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Preface

This report constitutes the mid-term report for the EU project “Quantitative Measurement of Aerosol Deposition on Skin, Hair and Clothing for Dosimetric Assessment” under the Nuclear Fission Safety RTD Programme, contract FI4PCT950019.

The project involves two partners: Imperial College from the UK and Risø National Laboratory from Denmark. The two partners have, for more than a decade, worked together on experimental research dealing with indoor aerosol. The technique with monodisperse particles labelled with neutron activatable tracers was developed in close collaboration at the end of the 1980’s for measuring indoor aerosol deposition velocities. Under the current contract the developed technique is being used to study the deposition to human body surfaces, such as skin, hair and clothing.

As a supplement to the original technique, Imperial College has developed a fluorescence scanning technique that has been used to study the particle-skin morphology and clearance from skin. Risø has made a dose model based on the parameters obtained during the project.

Both the partners in the project also participate in the EU Dermal Exposure Network (subgroups 4 and 5) dealing with surface contamination and source apportionment. Here the partners have gained useful knowledge from, for instance, dermatologists, and hope to disseminate the results to a wider forum.

The support of NRPB in the UK for financing an extra PhD student at Imperial College is acknowledged.

1 Objectives

A release of radioactive particles and gases from a nuclear installation will give rise to radiation exposure to workers and the surrounding population. In modelling of prospective accidents and dose reconstruction for past accidents, inhalation dose and dose due to external gamma radiation from the plume and from ground deposits are conventionally considered as the primary pathways at the time of the release. Deposits on skin of particles and reactive gases containing β -emitters will cause a dose to the skin and deposits on skin, hair and clothing will cause a γ -dose to the body. This contribution has so far largely been ignored in the estimates of total dose in accident consequence calculations, but in a recent article by the NRPB in EUR 13013 (Jones 1991) - The Importance of Deposition to Skin in Accident Consequence Assessments - calculations of the possible effect of a range of deposition velocities to the skin are presented. The paper states "The predicted expectation value of early deaths increases by about an order of magnitude over the range of deposition parameters considered here for a large accidental release." The paper contains a plea for experimental investigations into the processes of deposition to skin. Under an earlier contract the question of aerosol deposition to skin was addressed in a preliminary manner as part of a wider investigation concerning deposition of aerosol indoors. The initial measurements of deposition velocities to skin showed significantly higher values compared to those to passive surfaces such as walls of a room - this unexpected result has added to the importance of the present research. Thus previous work (including NRPB work) has highlighted three aspects of aerosol deposition to human surfaces: the radiological importance; unexpected high provisional deposition velocities and the complexity of the physics involved in the deposition and retention process. Particle retention by skin is a sampling issue in deposition and clearance studies. The kinetics of absorption and retention of a range of particles can be studied using animal and human skin in an in-vitro system currently established in the Imperial College Medical School. This in-vitro system has been shown to maintain the skin in a viable state and to provide an accurate and representative model of the in-vitro absorption of chemicals.

Drawing on previous developments in the generation of surrogate tracer aerosols, four research objectives have been identified in order to clarify the size and dosimetric effect of aerosol deposition on human body surfaces. These are:

1. Studying the physics of retention and sampling of particles from skin, hair, and clothing.
2. Measurement of deposition velocities to skin, hair and clothing, taking account of the wide range physical mechanisms (surface type, air flow, heating, electrostatics, etc.).
3. Estimating clearance rate of deposits from skin, hair and clothing: Natural clearance and forced clearance(e.g. decontamination)
4. Calculation of dose resulting from deposition at human body surfaces.

2 Progress in each work package

Consistent with the important physics outlined in the objectives above four work packages have been defined. The first three work packages deal with experimental work needed to establish the appropriate measurement protocols, understanding the processes and obtaining the relevant parameters for modelling. The last work package deals with the radiological modelling of the doses to man from aerosol deposition to the human body. For each work package a series of research tasks was defined and the subsection structure roughly follows the work tasks outlined in the work programme.

The extensive collaborations between the partners in former collaborative projects has provided the ability to label, with sensitive stable (neutron activatable) tracers, aerosols from the sub-micron (from 0.1 microns upwards) to supra micron (from 20 microns downwards) sizes and to undertake clearance studies using fluorescent tracers. These experimental abilities are supported by the facilities available at both centres; aerosol laboratories, aerosol test chambers (capable of stimulating medium size rooms) test houses, wind tunnels and a nuclear reactor at each partner's establishment - to allow stable tracer neutron activation analysis (NAA).

The general experimental technique using neutron activatable tracers have been described thoroughly in several joint publications, including the production, dispersion and sampling of tracer aerosol. Byrne *et al.* (1995) describes test chamber procedures and Fogh *et al.* (1997) describes experiments in houses. Briefly, aerosols with a well defined particle size are labelled with neutron activatable tracers that have a very low ambient concentration. These tracer particles are injected into rooms or test chambers and used to expose the objects of interest. By measuring the air concentration by air sampling and the surface concentration on the objects the exposure can be expressed as a deposition velocity. The aerosol deposition velocity, v_d , to indoor objects has been defined by Roed and Cannell (1987) as:

$$v_d = F / C_0$$

where F is the flux to the surface and is measured as the mass per area divided by the exposure time and C_0 is the reference air concentration measured in the centre of the room or test chamber. The deposition velocity is the most appropriate parameter for later modelling of the dose associated with exposure to a well defined release of particles.

In this project the objective is to measure deposition to human body surfaces such as skin, clothing and hair. Here the main experimental challenge is the retrieval of the deposited particles from the viable skin, whereas hair and cloth are simpler media as they can be bulk sampled. Sampling, together with retention on and clearance from skin is the topic of work package 1 (section 2.1). Work package 2 deals with issues concerning clothing and hair (section 2.2) and work package 3 deals with the deposition mechanisms. In section 2.4 the modelling of the dosimetric aspects of skin deposition is presented.

2.1 Sampling, retention, clearance issues for skin

This integrated work package includes an investigation of: sampling procedures from skin, the clearance of particulate from skin, contact transfer to skin, and in-vitro studies of the mechanisms of particle retention by and penetration into skin.

Sampling of particulate from skin

The measured values of aerosol deposition velocity on skin (as described in section 2.3) are underpinned by an accurate knowledge of the removal efficiency and consistency of the skin sampling procedure adopted. A summary of dermal exposure assessment techniques is presented in Ness (1994). The principal techniques which can be applied to the measurement of tracer aerosol particles on skin are (i) non-invasive optical scanning of the skin, exploiting fluorescent properties of the tracer particles (ii) skin wiping, (iii) skin rinsing or washing, (iv) tape-stripping of the skin's upper layers, (v) using air-currents to resuspend or suck particles from skin, (vi) sampling surrogate surfaces attached to the skin. Only invasive skin sampling protocols were seen as appropriate for the current work; as will be discussed in detail below, the current state-of-the-art of optical scanning systems is that only relatively high tracer particle levels can be detected. This has implications for surrogate surface sampling also: the degree to which a surrogate surface is representative of skin can only be tested in comparison with a non-invasive contamination detection method such as skin scanning, since any other method (such as wiping, for example) used as a comparison, has its own inherent sampling uncertainties.

Several invasive skin sampling strategies were tested for particle removal efficiency and consistency; experiments, both in-vitro and in-vivo, are described below. The data generated in these tests have an additional relevance for the current work: since invasive techniques remove particles from skin, information on removal efficiencies, and on the fate of the remaining particles, can be used in the design of strategies for skin decontamination, following an accidental radioactive release to the atmosphere.

In-vivo experiments

As described in more detail in the section on test chamber experiments, 4.5 μm neutron activatable tracer labelled aerosol particles were injected into a test room which housed a human volunteer with exposed forearms. After 45 minutes, during which the aerosol was allowed to settle, the volunteer was removed from the test room, and strips of cosmetic hair-removing wax were then applied to the arms. Five exposures were carried out, and in each case, six wax strips were used. For comparison, other areas of the arms were wiped, with fabric wipes (60% cotton, 40% polyester, 2.5 cm^2), moistened with de-ionised water. No measure of the absolute deposition flux to the arms (which would require a non-invasive method) could be made in these measurements, so that it is not meaningful to quote a wiping or waxing efficiency. However, it could be seen that the coefficient of variation between samples was 28% in the case of waxing, and 21% in the case of wiping.

To determine quantitative skin wiping efficiency, the approach taken was to expose excised skin to neutron activatable particles, but then to fix this skin to a human volunteer during the wiping process. This would ensure that the skin was wiped with similar pressure to that exerted in wiping the human volunteers' own skin, and therefore, the study can be considered as, effectively, an in-vivo one. Sections of shaved rat skin were placed (on ice, to prolong viability) in an aerosol exposure chamber, and exposed to 4.5 μm particles for one hour. The skin sections were then halved and one side was fixed, exposed side upwards, to the back of the (gloved) hand of a human volunteer. The rat skin was then consecutively wiped with five fabric sections, which were moistened with de-ionised water. The wipes and the skin, both wiped and unwiped, were analysed, and particle removal efficiencies in the range 15-40% were recorded.

The relative particle mass collected on the five wipes is shown in Figure 2.1, and it can be seen that particle recovery decreases with each subsequent wipe.

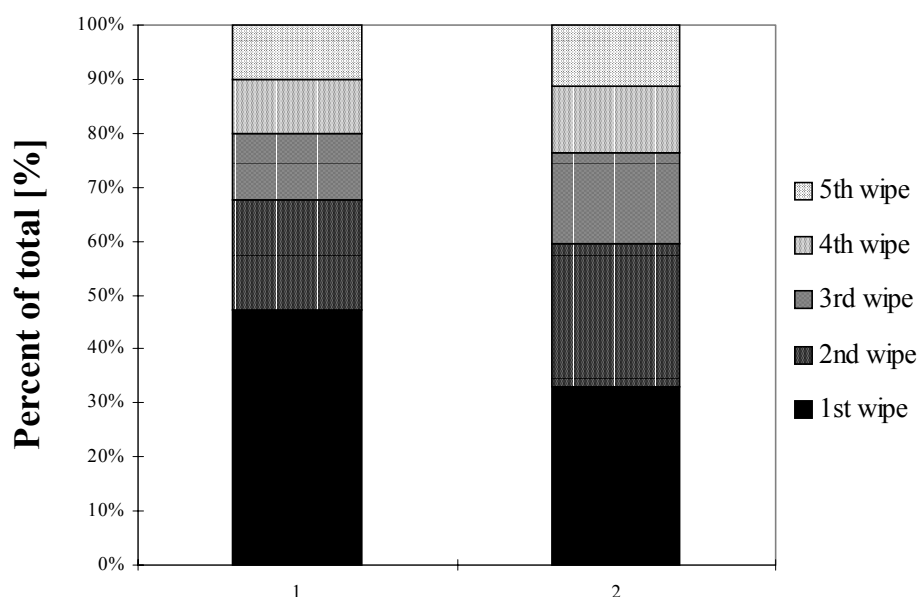


Figure 2.1 Histogram, showing the relative particle recovery on five consecutive wipes of skin exposed to 4.5 μm particles

A similar pattern can be seen for 0.5 and 2.5 μm particles on Figure 2.4 and 2.5 showing three consecutive wipes after an exposure in a house. However, analysis of the wiped skin itself indicated a significant quantity of residual tracer, suggesting that there exists a dislodgable fraction, the distribution of which may or may not be modified by the wiping process. In Table 2.1 the relative distribution of recovered tracer by three subsequent wipes can be seen. The relative recovery of 0.5 μm particles by the first wipe (73 % of total) was higher than for 2.5 μm particles (66 % of total). This difference was significant ($p = 0.02$, $n = 37$).

Table 2.1 Tracer recovery on three subsequent wipes.

	No. sample locations	1 st wipe [%]	2 nd wipe [%]	3 rd wipe [%]
0.5 μm particles	37	73 \pm 15	17 \pm 8	10 \pm 9
2.5 μm particles	58	66 \pm 17	21 \pm 11	13 \pm 11

In order to investigate the influence of the size of the sampled area on the amount of recovered tracer, different sized areas were wiped. In one experiment 8 cm^2 areas were wiped on the arms and 100 cm^2 areas were wiped on the chest and back of a volunteer. It was found the amount of tracer per unit area was very similar for the two different area sizes: 18 \pm 9 ng cm^{-2} versus 23 \pm 13 ng cm^{-2} for the 0.5 μm particles and 5.5 \pm 2.8 ng cm^{-2} versus 5.2 \pm 2.8 ng cm^{-2} for 2.5 μm particles. As sufficient tracer could be detected on an 8 cm^2 area, it was decided to use this smaller area in future tests as this area could be better controlled with a metal template when wiping (as described in the sampling protocol in the Annex 7.1). Also using a smaller area enables sampling to be carried out on a wider range of well defined body parts.

Sampling efficiency

In order to determine quantitative tracer efficiencies, aerosol exposure of skin was carried out in a small (0.048 m^3) test chamber. The skin used in these experiments was hairless rat skin, chosen since it has a hair follicle density similar to human skin. The skin was cut into 1.7 cm diameter circles and throughout the aerosol exposure period, was kept viable by floatation on an appropriate receptor fluid.

Quantitative sampling efficiencies were determined using skin exposed to neutron-activatable particles, and then subjected to the following particle sampling strategies: (i) an area of skin was wiped five times (ii) skin sections were pressed, exposed side down, on strips of cosmetic hair-removing wax, and then removed from the wax with tweezers (iii) skin samples were placed individually in jars filled with de-ionised water, and shaken vigorously for thirty seconds. It should be noted that the waxing and wiping procedures used were chosen to imitate those used in the in-vivo experiments, described earlier. The skin, wipes, wax, etc. were all analysed by NAA and Table 2.2. shows the mean removal efficiencies, with associated variation, of 2.5, 4.5, 8 micron particles from skin (one hour exposure)

Table 2.2 Removal efficiencies for different sampling methods.

Particle Size	Wiping eff. [%]	Waxing eff. [%]	washing eff. [%]
2.5	72.5±8.8	75.8±3.0	31.5±6.3
4.5	71.1±8.1	77.0±14.7	36.3±4.2
8	76.4±5.3	68.0±9.9	35.7±4.1

The effect of skin wiping on removal and redistribution of particles was studied using skin which had been exposed to fluorescent tracer labelled particles, for periods varying from 30 minutes to 5 hours. In this case, the skin sections, after particle sampling, were submerged in paraformaldehyde (to stop metabolic activity), dehydrated, embedded in paraffin wax, and then cut into 5 micron sections and examined under the fluorescent microscope. These results will be discussed in the section on particle retention below.

Based on the results shown in Table 2.1, washing was neglected as a skin sampling strategy for the current work, due to its low efficiency, and the anticipated difficulties in flowing liquid over a controlled area of skin. The wiping efficiency determined by using shaved rat-skin “in-vivo” was not considered to be reliable, due to the large number of hair follicles involved, relative to human skin; the merit of this experiment lies in the fact that it indicates that there is a dislodgeable fraction of particulate material on wiped skin, which is borne out in the in-vitro exposures of skin to fluorescent particles (discussed later). Although the in-vitro experiments, with hairless rat skin and neutron activatable particles, indicate that washing and wiping had similar sampling efficiencies, it was observed that the variability associated with wiping is lower, and a similar observation was made in the in-vivo study. For these reasons, skin wiping was adopted as the preferred sampling strategy for the current work, and details of the wiping protocols are presented in Appendix 7.1.

Retention and clearance of particulate from skin

For dosimetric assessment and decontamination, it is important to understand how particulate penetration, and removal efficiency, is influenced by the duration of skin exposure to the particles. As has already been indicated above the skin has a unique surface and is therefore likely to exhibit very specific behav-

behaviour in terms of particle retention, which must be understood for radiological risk assessment. Studies aimed at understanding the time-course of particle removal from skin, both through active cleaning, and by the particles simply falling away during normal human activities are described below. Penetration of toxic particles below the skin's outer surface layer has the dual effect of exposing deeper layers of the skin and making the particles difficult to remove by any external means. The section on in-vitro studies describes experiments aimed at understanding the particle size dependence of dermal penetration rate, and also the influence of particle residence time on the skin. The relationship between skin wiping and skin penetration is also discussed in this section.

Fluorescence scanning system

In order to follow the time-course of particle removal from human skin, since that surface cannot be readily removed for analysis, it was necessary to develop a non-invasive analysis system. Fluorescence scanning has been applied to the study of dermal contamination by several researchers, notably Fenske *et al.* (1996) and Roff (1994), and the main components of their systems were an array of filtered lights, for illuminating a tracer aerosol, which had optimal fluorescence in a narrow wavelength range, and a filtered CCD camera, with image processing software, for collecting and analysing the fluorescence.

A review of the literature revealed that most earlier studies focused on the visualisation of highly fluorescent liquids under ultra-violet illumination. Design considerations for the present study took into account the significantly smaller masses of tracer which would be available as solid particles in the present work, than were available as liquids in other work, and the fact that the skin has an inherent fluorescence under ultra-violet illumination, which would be likely to interfere with the signal from the expected low particle concentration on the skin. Therefore, it was decided that a system would be developed which would rely on visible illumination. Fluorescein was the tracer chosen for the work, and the particles were dyed using a process described by Hodson *et al.* (1994). The components of the fluorescence scanning system are described in detail in Annex 7.2.

Before it could be used in clearance studies, it was necessary to calibrate the fluorescence scanning system i.e. to determine the electronic signal associated with a known mass of tracer-labelled particles. The system was calibrated by suspending several samples of weighed tracer labelled silica in liquid water, and using a Buchner apparatus to evenly distribute the suspended material on filter papers. The dried filter papers were then analysed with the fluorescence scanning system, and a linear correlation ($R = 0.97$) between mass of tracer and fluorescent signal was obtained. An estimate of the limit of detection of the system was made: $2.5 \text{ mg of tracer particles cm}^{-2}$; this is significantly higher than the limit of detection of neutron activation analysis.

Experiments were carried out, whereby $4.5 \text{ }\mu\text{m}$ particles were applied to the forearms of volunteers by shaking the particles close to the skin and then removing the un-adhered fraction by gentle blowing. This approach was adopted since the limit of detection of the scanning system would have required that volunteers spent long periods in a test chamber if the arms were to be exposed by direct deposition. It was considered that localised application of tracer particles to the arms would represent a "worst case" scenario, from the point of view of clearance, since particle adhesion to the skin could not be lower, and might even be higher, than if deposition from ambient air had occurred. The level of loading of tracer particles on the skin was of the order of 40 mg cm^{-2} .

Approximately five minutes after exposure to particles, the volunteers' arms were rinsed with cold water. Tests were carried out on several different volun-

teers, with varying degrees of arm hair and the results showed that, in all cases, a single rinsing reduced the level of tracer on the arm to below the limit of detection (2.5 mg cm^{-2}), indicating that the removal efficiency of cold water rinsing is greater than 90% for $4.5 \mu\text{m}$ particles. It should be noted that this value is considerably higher than the rinsing efficiency determined in the in-vitro studies presented in Table 2.1. where the particles resided on the skin for one hour before removal. The discrepancy between the values may indicate that particle removal efficiency is a function of residence time on the skin; further evidence of this is presented in the next section.

Other studies were carried out whereby volunteers were exposed to $4.5 \mu\text{m}$ tracer particles, allowed to conduct their normal activities (ranging from sedentary indoor work, to outdoor walking) and were analysed at two hour intervals. In each case, one of the volunteer's arms was treated with cosmetic moisturising cream (at a level thought to be representative of actual use), prior to particle loading. Figure 2.2 shows the pattern of clearance of particulate from the arms of two volunteers, one with little arm hair (MB) and one with significant arm hair (KB). The less hairy individual participated in some outdoor activity, in windy conditions, during the study period, while the hairier subject remained indoors. The results indicate that the residence of particles on the skin was influenced by the volunteer's arm hair concentration and the type of activity. This finding has important implications for persons unwittingly exposed to radioactive particles, and who do not take steps towards active decontamination. The use of moisturiser on the skin was not found to significantly influence particle retention.

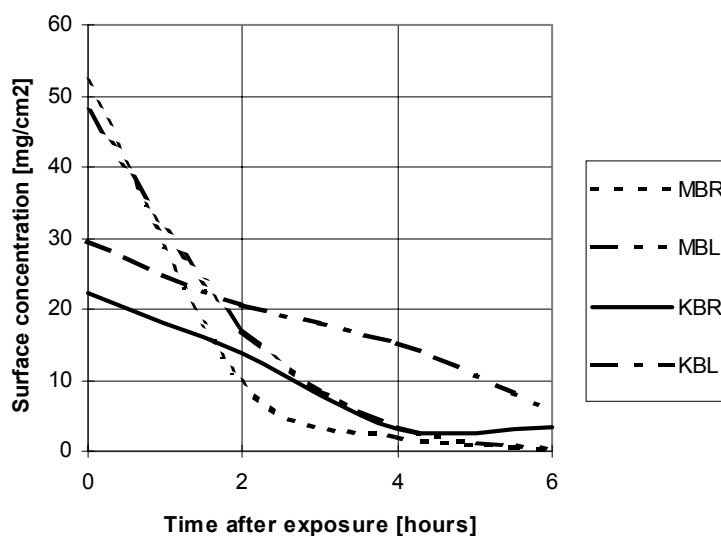


Figure 2.2. Curves showing the variation in particle loading on the arms with time, for two volunteers (MB and KB) on the right (R) and left (L) arm.

It should be noted that the clearance half life for particles, which can be deduced from Figure 2.2, i.e. a few hours, is appreciably shorter than that used in accident consequence codes such as COSYMA. Since, the clearance half life is a critical parameter in the dosimetric assessment, it is considered important to elaborate on the limited experiments reported here, in order to obtain more information about clearance from skin.

In-vitro studies.

Using an identical procedure to that described earlier in this section, hairless rat skin samples were prepared and exposed to fluorescent particles. Three particle

sizes were used, with nominal aerodynamic diameters of 2.5 µm, 4.5 µm and 8 µm (these were the same particles which have been used for the deposition velocity measurements described in this report and elsewhere). The skin was exposed to each particle size for two time-periods: 30 minutes and 5 hours.

A selection of results is shown in Plates 1-3. As can be seen in Plate 1, after 30 minutes, the 2.5 µm particles were distributed all over the stratum corneum and the hair follicles. Both the 4.5 µm particles and the 8 µm particles (not shown) were distributed over the stratum corneum, with the 4.5 µm, but not the 8 µm particles, exhibiting a tendency toward the hair follicles. As Plate 2 illustrates, after a five hour exposure, the 2.5 µm particles had penetrated deeper into the hair follicles. The 4.5 µm particles (not shown) had penetrated to a lesser degree, and the 8 µm particles (not shown), while now tending towards the hair follicles, had not penetrated. These results indicate that particle size and residence time on the skin are both important determinants of particle penetrability, and hence, susceptibility for clearance; i.e. once the particles are below the skin surface their removal by external means becomes difficult.

Plate 3 shows wiped skin, which had had prior exposure to 2.5 µm particles for 5 hours. Comparison of this with Plate 2, which is a representation of a skin sample with an equal particle exposure time, indicates deeper penetration of the particles on the wiped skin, suggesting that the wiping process, although removing significant quantities of particles, may promote follicular penetration of particles. It may be concluded, therefore, that while wiping is an effective dermal exposure assessment technique, its effectiveness as a dermal decontamination strategy is compromised.

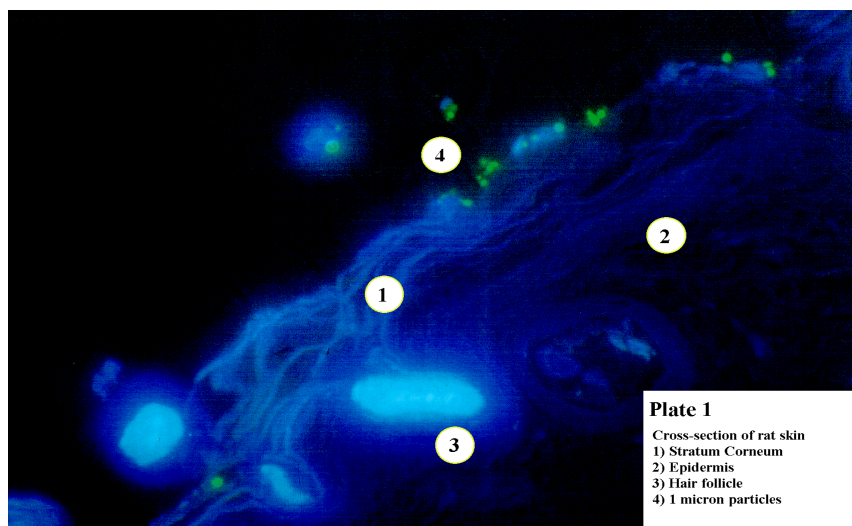


Plate 1 2.5 micron particles on skin for 30 minutes

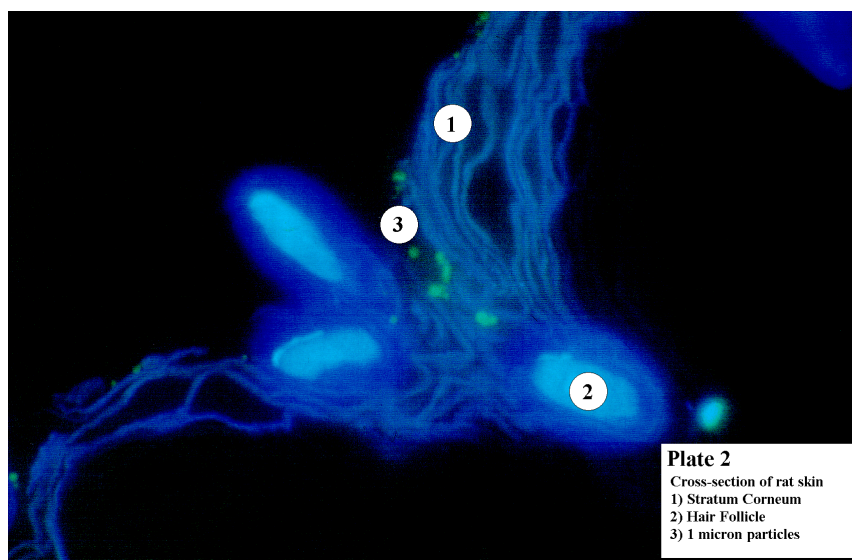


Plate 2 2.5 micron particles on skin for 5 hours

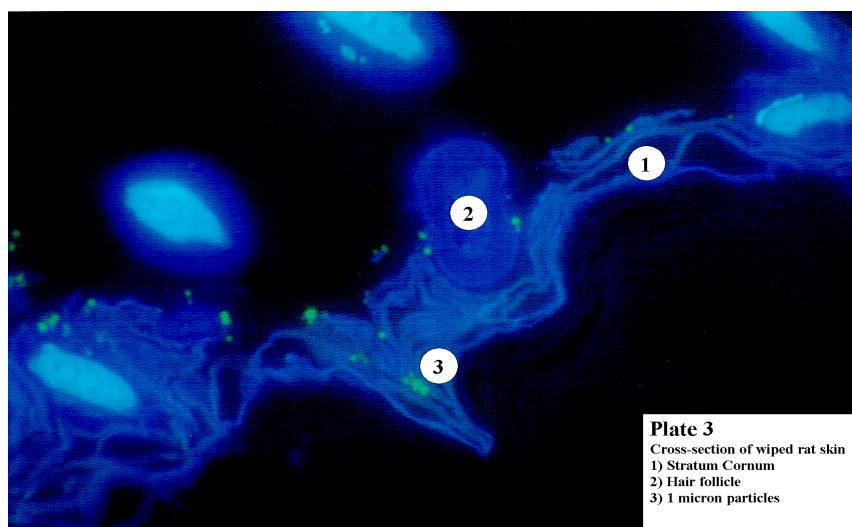


Plate 3 2.5 micron particles on skin for 5 hours, and skin then wiped

2.2 Sampling, retention and clearance issues for clothing and hair.

In this section, dealing with work package 2, the issues of deposition to clothing and hair, together with retention on cloth will be discussed corresponding to the work package subsections 2.1, 2.2 and 2.3 in the technical annex of the contract. The two last issues belonging to this work package, “clearance from hair” and “depth profile of deposits”, will be resolved in the final report as scheduled in the original work programme

The use of aerosol labels which can be analysed by neutron activation analysis, means that the highly sensitive analysis of deposition and retention on clothing and hair is straightforward as hair and most clothing materials have a low background when exposed to neutrons. Thus, samples cut from clothing and hair can be analysed readily using neutron activation analysis, by analysing bulk samples.

Deposition to clothing

In order to make deposition experiments a protocol for exposing and sampling the clothing is needed. The protocol for clothing sampling is simple, and is as follows:

1. A suitable air concentration of tracer particles is established in a room or test chamber as described in the beginning of Chapter 2. The particles will be of known size and the integrated air concentration is determined by air sampling.
2. The volunteer, wearing a selected clothing material, is exposed to tracer aerosol. The material should be test activated in a nuclear reactor beforehand to ensure that the background noise from trace elements in the cloth is sufficiently low to enable good detection of the tracer particles.
3. Using clean scissors, an unexposed individual wearing gloves, cuts sections (approximately rectangular) from the clothing.
4. The position of the sample is measured, with respect to the shoulder of the garment in the case of a sleeve sample, and with respect to the neck of the garment in the case of a sample from the chest/back area.
5. The clothing sample is conveyed, with forceps, to a clean, labelled plastic bag.
6. The area of the sampled clothing is measured (samples are typically 10 to 20 cm²).
7. The tracer content is determined by irradiating the entire sample in a nuclear reactor.

Using the protocol above, a series of clothing samples were obtained during test chamber experiments in the UK and under real life conditions in Denmark. In Table 2.3 there is a review of the deposition velocities obtained. It is interesting to note that even though most of the samples were mounted in the vertical position on the chest and back of human volunteers, the deposition velocity is increasing with particle size, suggesting that inertial effects play an important role in the deposition process. The deposition velocities for 0.5 µm particles found in the test chamber were much higher than those found in the office and house environments, but it should be noted that a different kind of clothing fabric was involved. It be seen that the roughly woven jumper having the largest surface area also had the highest deposition velocity and this is good agreement with the expected behaviour.

Table 2.3 Review of deposition velocities obtained for clothing.

Experimental site	Type of Cloth	Number of samples	Deposition velocity [10^{-4} m s $^{-1}$] for particle size		
			0.5 μ m	2.5 μ m	4.5 μ m
Office 6	Thick cotton	12	0.11 \pm 0.02	1.7 \pm 0.2	
Office 7	Thick cotton	12	0.91 \pm 0.52	4.5 \pm 1.3	
RH21	Thin cotton	6		4.4 \pm 0.4	
Test chamber	Jumper	12	22.0 \pm 1.2		35.0 \pm 1.3
Test chamber	Shirt	12	12.0 \pm 0.5		19.0 \pm 0.6

A sampling protocol for hair and some results

Whereas sampling of hair is as straightforward as cloth sampling some problems are associated with determining the projected area of a hair sample. Two different approaches have been used to solve this problem, as outlined below.

At Risø a sampling protocol for hair involving a complete hair cut have been utilised. The hair cut is performed in several stages, splitting the samples into inner and outer layers, so that an estimate of the depth profile of aerosol deposition can be made. The area of the test person's scalp is used as the deposition area. The major disadvantage of this approach is the long interval after sampling for which one must wait until the test persons hair will allow further sampling. Also, in the experiments carried out, no longhaired persons have volunteered for a full hair cut.

At Imperial College, experiments have been carried out using full hair wigs, which are entirely sampled. After sampling the wigs are ashed before analysis. With this sampling strategy, sampling can be performed for as long as the wig supply continues. The major uncertainty about the procedure is the question of whether the wigs are representative of human hair. Experiments have also been carried out at Imperial College whereby volunteers, while wearing swimming caps, were exposed to tracer particles; this was to simulate the case where an exposed person might have no head hair.

Table 2.4 presents the results of the hair deposition experiments. It can be seen that the deposition velocities for 2.5 and 8 μ m particles are approximately 50 % higher than those presented in Table 2.3 for clothing. The deposition velocities to the swimming caps were as high or higher than those to the wigs. This is unexpected as the wigs have a much larger surface area for deposition, but could be a plausible result if surface charge effects are considered as discussed in section 2.3. The result of the first full hair cut experiment was similar to that for wigs and caps for the larger particles, but a very high deposition velocity was found for the 0.5 μ m particles; this result needs to be verified with more experiments.

Table 2.4 Deposition velocities to hair

Deposition velocity 10^{-4} m s $^{-1}$	Particle size [μ m]		
	0.5	2.5	8
Wig	25.0 \pm 1.2 (18)		34.0 \pm 1.1 (20)
Cap	26.0 \pm 2.1 (8)		53.0 \pm 4.8 (10)
Full hair cut	126 (1)	31 (1)	
1			

Clearance from clothing

Clothing contaminated with radioactive particulate may give rise to an external radiation dose to the wearer both initially and during subsequent re-wearing, if cleaning practices used were inefficient. The efficiency of particulate removal from clothing was investigated, using neutron-activatable tracers.

Firstly, particle clearance during normal wear of clothing was studied by sampling at appropriate times during normal activity (i.e. walking around while wearing contaminated clothing). Samples arising from these experiments are still being analysed.

Secondly, the decontamination effect of domestic washing procedures using washing machines has been studied in several experiments. Exposed pieces of cloth were cut into two pieces. One was washed and the pair was then activated so that the tracer contents could be compared. In Table 2.5 the results from three exposures can be seen. The Office 6 and 7 exposures occurred to two people wearing laboratory coats while sitting in an office, reading. 6 cloth pieces were sampled from each person and divided into two parts. The RH21 result, was obtained by cutting samples from a T-shirt worn by a human volunteer in a room and the last two rows are for garments worn by test persons sitting in a test chamber. Generally, the smaller particles are more difficult to remove than the larger particles, suggesting that small particles will adhere better to the microstructures of the cloth, as can be seen in Table 2.5. The jumper was seen to be easier to clean than the cotton materials. Even though the curly macrostructure made the jumper have a higher aerosol deposition velocity than the cotton, the microstructure of the jumper was probably smoother as it was acrylic, thus explaining the lower adhesion of particles.

Table 2.5 Review of clearance from cloth of particles by domestic washing machines.

	Type of Cloth	Number of Pairs	Reduction efficiency for particle size		
			0.5 μm	2.5 μm	8 μm
Office 6	Thick cotton	12	0.80 \pm 0.22	0.60 \pm 0.12	
Office 7	Thick cotton	12	0.73 \pm 0.24	0.70 \pm 0.10	
RH21	Thin cotton	6	-	0.27 \pm 0.20	
Test Chamber	Jumper	12	0.31 \pm 0.07		0.11 \pm 0.02
Test chamber	Shirt	12	0.65 \pm 0.16		0.15 \pm 0.03

In Figure 2.3 the combined clothing washing results from the Office 6 and 7 tests are been presented together for the two different particle sizes, 0.5 and 2.5 μm . The amount of tracer after washing is presented as a function of the amount of tracer before washing on each sample. For both types of particles it seems that there is an approximately linear relation between the tracer amounts before and after washing, implying a constant decontamination factor, which is independent of particle loading and sample position. The fact that a regression line can be drawn with a zero intercept verifies that there is no tracer background or any non-removable fraction in the material tested.

$$v_d = \frac{\text{Tracer mass deposited}}{\text{Average air conc.} \times \text{Exposure time} \times \text{Wiping efficiency}}$$

where the tracer mass deposited is determined by subsequent wiping, the average air concentration is determined by filter sampling, the exposure time is the residence time of the test persons in the test room and the wiping efficiency correction is taken from section 2.1 and is 0.73.

Test chamber measurements.

Extensive measurements of aerosol deposition on the body, under simulated indoor conditions, have been carried out using a 32 m³ test chamber. The experimental procedure essentially involved a human volunteer(s) entering the test chamber after tracer aerosol had been released and well-mixed by other personnel, and remaining there for up to 45 minutes. Aerosol concentration measurements were made via a dichotomous aerosol filtration system at the centre of the test room. A small fan was used throughout the aerosol mixing period, and remained running during the deposition interval, but care was taken to ensure that the volunteer was not seated in the direct path of the fan, and that impaction of particles carried by the fan did not significantly contribute to the flux to the body.

In most cases, the volunteer remained seated in the chamber throughout the experiment, and the only movement was that necessary to change the air filters. Following the aerosol deposition period, the volunteer left the test chamber and wipe samples were taken from the forearms, and in some cases, from the face, as described in section 2.1.

Using three aerosol particle size distributions, 2.5, 4.5, and 8 µm, in excess of 50 individual volunteer exposure events were carried out, resulting in 176 skin wipe samples. Table 2.5 presents the measured aerosol deposition velocities, averaged over all samples. Statistical analyses were carried out to ascertain whether there was a significant difference between deposition velocity to the arm and face of an individual volunteers; no difference was found. Neither was there a significant difference in deposition velocity to the arms of different volunteers (who had different levels of arm hair).

Table 2.6 Measured aerosol deposition velocities to skin; data (means and standard deviations) derived from experiments involving three human volunteers.

Particle size	2.5 µm	4.5 µm	8 µm
Deposition velocity [10 ⁻⁴ m s ⁻¹]	15 - 19	137 - 151	192 - 219
No. of samples	20	114	42

In several of the tests, filter papers were attached to the walls and floors of the test chamber throughout the deposition period. These yielded the result that, for 4.5 µm particles, the average deposition velocities to the vertical and horizontal surfaces of the test chamber were of the order of 10⁻⁵ m s⁻¹ and 10⁻⁴ m s⁻¹, respectively. As can be seen from Table 2.6, relative to these values, aerosol deposition velocities to the skin were found to be high and it was therefore considered to be of interest to examine the influence on deposition velocity of some of the individual factors characterising the human body: electrostatics, heat, and surface roughness.

Determination of aerosol deposition velocities by skin wiping, as described earlier, incorporates issues of deposition on surfaces of different roughness, but also issues of retention of material to a different degree when these surfaces are wiped. As stated earlier, no significant difference was observed between aerosol deposition velocities on hairy and non-hairy volunteers, which may indi-

cate that enhanced deposition promoted by increased roughness may be concealed by difficulty in removing aerosol from rougher surfaces (alternatively, it may indicate that another skin-related factor is more significant than roughness). For this reason, in order to fully understand the dependence of aerosol deposition velocity on surface roughness, it is instructive to measure direct deposition on surfaces of varying roughness attached to the skin. This was achieved by attaching small squares (typically 12 cm²) of felt, plastic and polythene to the forearms of the volunteer by means of adhesive spray. The volunteer was then exposed to aerosol as previously described, and the samples were removed for analysis after an appropriate deposition period. In some cases, a heated aluminium cylinder 1.5 m high and 0.15 m diameter, to which felt, polythene and filter paper samples were attached, was also present in the test chamber. The cylinder had the advantage of a greater surface area, relative to the human arm, on which to mount samples, so that possible differences in aerosol deposition due to spatial variability could be averaged out in a large number of samples. Also, the cylinder was completely immobile so that any effects due to aerosol deposition via impaction on samples attached to the human body could be eliminated.

Aerosol deposition velocity measurements were made with three particle size distributions: 2.5, 4.5 and 8 µm; the cylinder was only present in the test chamber for those experiments involving 2.5 and 8 µm particles. The data are shown in Table 2.7. Statistical tests showed that there was no significant difference between aerosol deposition to samples attached to the arm and to the cylinder, and data derived from both bodies are therefore shown together in Table 2.6. It can be seen that while aerosol deposition to felt is greater than to smoother filter paper, the greatest deposition velocity was observed to the smoothest surface: polythene (although statistical analysis showed that the difference between deposition on felt and plastic is not significant at the 95% confidence interval for 8 µm particles). This indicates that another factor associated with plastic surfaces- electrostatic charge- is an important modifier of aerosol deposition.

Table 2.7 Cylinder experiments. Deposition velocities for three different surface types mounted on a cylinder. The 95% confidence intervals are quoted with the number of tests in parenthesis.

Deposition to surface types	Particle size [µm]		
	2.5	4.5	8
Filter paper [10 ⁻⁴ m s ⁻¹]	1.1-1.4 (16)	5.7-8.4 (8)	13-21 (18)
Felt [10 ⁻⁴ m s ⁻¹]	2.6-4.0 (16)	19-23 (33)	31-43 (18)
Polythene [10 ⁻⁴ m s ⁻¹]	4.0-7.1 (16)	24-36 (39)	31-51 (18)

Electrostatic charge may be generated by tribo-electrification of both footwear and clothing (Greason 1994) and is held by the insulating qualities of the clothing and skin (Grandolfo *et al.*, 1985). Aerosol transport theory suggests that electrostatic charge influences aerosol deposition, particularly for the smaller particle sizes, but the relevance of this information for the present work is unclear since little quantitative data are available on charges on the human body (it is known, however, that electrostatic charge on the body is highly variable). No attempt was made in the current work to improve this, but experiments were simply carried out to determine the difference in aerosol deposition velocity to skin which was held at electrical ground potential, and skin which was at "normal" potential. An elastic electrical conducting strap, of the type used by computer repair personnel, was attached to one wrist of a volunteer, and the other end of the strap was connected to the wall of the laboratory. As

before, the volunteer was exposed to tracer aerosol (4.5 μm particles) and both the grounded and ungrounded arms were then wiped. The experiment was repeated six times, with the conducting strap alternated between the volunteer's arms. The result is shown in Table 2.8.

Table 2.8 Review of experiments testing electrostatic effects on the deposition process for 4.5 μm particles.

	No. of tests	Grounded arm [10^{-4} m s^{-1}]	“Normal” arm [10^{-4} m s^{-1}]
Deposition velocity	6	81	136
Standard deviation	6	3	7

Another mechanism suspected to be responsible for the high magnitude of aerosol deposition (relative to internal building surfaces) on body surfaces was convection caused by the heat of the human body. Using neutron-activatable tracers and the heated aluminium cylinder as in the present work, it was observed by Bell (1994) that heating the cylinder to human body temperature resulted in enhanced aerosol deposition on the cylinder's surface. Nazaroff and Cass (1987) postulated that when a flat vertical plate is heated, particle deposition is likely to be enhanced when the characteristic surface roughness is less than the concentration boundary layer caused by thermophoresis. It was calculated that for a particle diameter of 3 μm and an air-surface temperature difference of 10K, the concentration boundary layer close to a surface is of the order of 0.5 mm, significantly less than the likely roughness height of the human body. Enhanced aerosol deposition on the human body cannot therefore be easily explained by thermophoresis, but is more likely to be attributable to turbulence generated by convective currents. Fluctuations in aerosol concentration due to turbulence in proximity to heated human phantoms have been reported by Parker *et al.* (1990).

In the present work, it was not possible to measure aerosol concentration fluctuations close to the body of a human volunteer, but measurements of air velocity with distance from the body were made, using hot-wire anemometers. It was found that the maximum air velocity occurred near the chest of the volunteer, and was 0.25 m s^{-1} , falling to 90% of this value at a distance of 20 mm. This finding is in good agreement with the observations of Homma and Yakayima (1988), who used infra-red thermography to visualise the thermal envelope around the body.

Realistic environments

Aerosol deposition experiments involving human volunteer have been carried out at Risø in office environments and under domestic conditions. In order to permit detailed examination of the variability of the data it was decided to work with only two particle sizes: 0.5 μm indium particles and 2.5 μm dysprosium particles.

The results of the first two office experiments was presented in the report of an earlier EU contract. Here results are presented from an additional 5 office experiments. In each office experiment the same two male test persons were exposed. The persons entered the office after a well mixed tracer concentration was established and a third person in the test room took care of the particle dispersion, air sampling, wind velocity measurements, etc. A fourth unexposed person made the skin wipes in a neighbouring room after the test. The length of the exposure was varied in order to allow plotting of the recovered amount of tracer as a function of the integrated air concentration. In two of the tests (Of-

fice 4 and 5) one of test persons was working at a PC (KGA) and the other person was reading. In the two other tests (Office 6 and 7) both test persons were reading. Office 8 was a joint experiment between Imperial College and Risø and it was for the purpose of comparison of the experimental procedures used by the partners.

In Table 2.9 the deposition velocities found in the six different tests are presented. For the four office experiments, results are presented for the two test persons are presented individually, and as an overall average. It can be seen that the results for KGA were similar regardless of whether or not he was sitting in front of a PC. For the 0.5 μm particles there was a slight increase in deposition velocity from 0.00023 to 0.00034 m s^{-1} , but this was not significant ($p = 0.15$ in a t-test). For the 2.5 μm particles there was no difference in the overall mean deposition velocity: 0.0040 versus 0.0040 m s^{-1} .

When the deposition to the two different test persons were compared it was found that the deposition velocity was significantly higher to KGA than to CLF. For the 0.5 μm particles the deposition velocity increased from 0.00013 for CLF to 0.00019 m s^{-1} for KGA and this increase of 46 % was significant ($p=0.004$). For the 2.5 μm particles the increase was 112 % from 0.0019 m s^{-1} for CLF to 0.0040 m s^{-1} for KGA and this increase was also significant ($p=0.003$). The main difference between the two test persons is that CLF has limited arm hair growth whereas KGA has rather hairy arms. This result has also been observed in previous experiments reported by Lange (1995), but the results obtained in the test chamber experiments indicated that arm hair concentration was not an important determinant of aerosol deposition velocity.

Table 2.9 Average deposition velocities for different persons in different tests.

	Number of sample locations []	Particle size	
		0.5 μm [10^{-4} m s^{-1}]	2.5 μm [10^{-4} m s^{-1}]
CLF	5	2.0 \pm 3.3	7.5 \pm 3.8
KGA (PC)	5	4.6 \pm 2.7	40.8 \pm 35.4
Office 4 average	10	4.0\pm2.3	24.1\pm29.6
CLF	5	0.8 \pm 0.3	16.3 \pm 5.6
KGA (PC)	5	2.3 \pm 0.9	38.6 \pm 15.4
Office 5 average	10	1.5\pm1.0	27.5\pm16.0
CLF	5	0.6 \pm 0.2	18.7 \pm 5.8
KGA	5	2.9 \pm 1.6	45.5 \pm 23.1
Office 6 average	10	1.7\pm1.6	32.1\pm21.2
CLF	5	0.4 \pm 0.2	32.6 \pm 8.8
KGA	5	1.8 \pm 1.9	34.2 \pm 24.3
Office 7 average	10	1.1\pm1.5	33.4\pm17.3
RH39 average	17	1.1 \pm 0.6	27.5 \pm 14.3
RH21 average	21	NA	19.6 \pm 19.8

In Figure 2.4 and 2.5 the results from the Office 6 test have been shown for the two particle sizes used. It can be seen that the deposition velocity is higher for the KGA test person (prefix 'K' to the right in the figures than to the test person CLF (prefix 'C' to the left on the figures). When the two diagrams are compared it can also be seen that the deposition pattern for the two different particle sizes are similar, that the minimum and maximum deposition velocities occurs at the same sampling locations. As discussed in section 2.1 the figures also illustrate that the most tracer is removed with the first wipe and the tracer level thereafter decreases with subsequent wipes.

In Figure 2.4 and 2.5 it can also be seen that there is a difference between upwards and downwards facing wiping locations on the arm. The suffix ‘U’ means under (or downwards) and the suffix ‘O’ means over (or upwards) and it can be seen that there is a higher deposition to the upwards facing location. This pattern was observed in most of the tests.

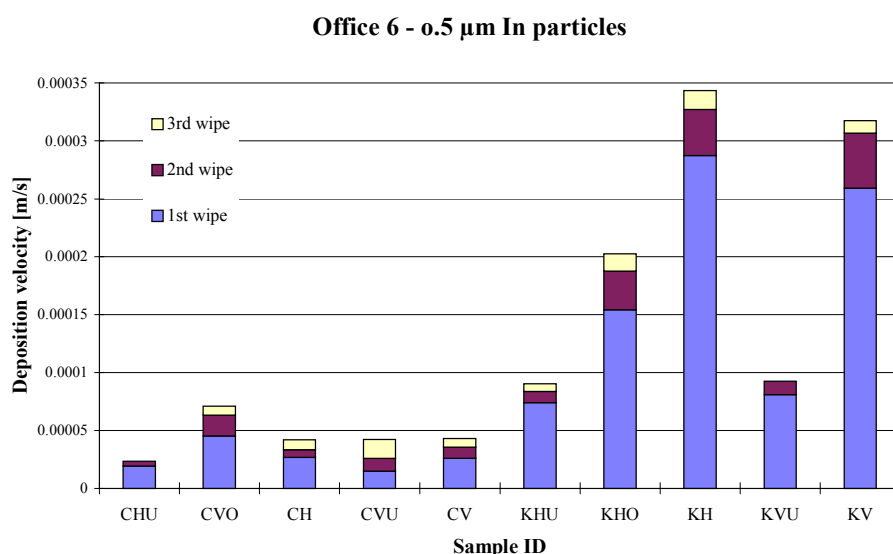


Figure 2.4 Deposition velocities for 0.5 μm indium particles obtained by three subsequent wipes on five location on two different test persons (CLF is prefix ‘C’ to the left and KGA is prefix ‘K’ to the right).

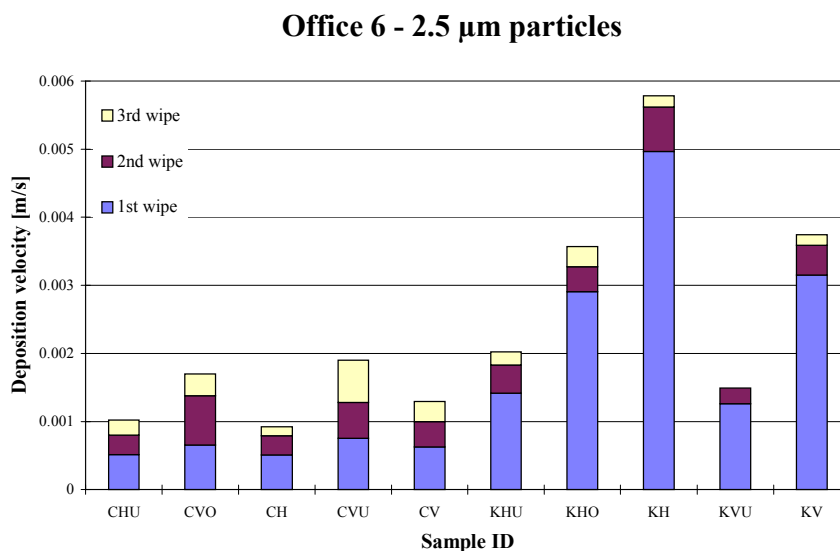


Figure 2.5 Deposition velocities for 2.5 μm dysprosium particles obtained by three subsequent wipes on five location on two different test persons (CLF is prefix ‘C’ to the left and KGA is prefix ‘K’ to the right).

In the two experiments in real houses (denoted RH39 and RH21), 5 different persons were exposed (a total of 10 different persons for the two tests), that had not previously participated in the skin wipe experiments. This was done in order to increase the sampling population. As can be seen in Table 2.8 the average deposition velocities found in the two house experiments were close to those determined in the office experiments.

In order to examine the relation between the integrated air concentration and the amount of recovered tracer, the exposure times and the amount of emitted aerosols was varied from test to test. It should be noted that the deposition velocity, by definition, is independent of the actual levels of exposure. The amount of recovered tracer (measured as tracer mass per unit skin area) was plotted as a function of the integrated air concentration (measured as tracer mass multiplied by sampling time and divided by sampled air volume) in Figure 2.6 for the 0.5 μm particles and in Figure 2.7 for the 2.5 μm particles. In this way it can be examined whether a linear relation between the integrated air concentration and the deposited tracer mass exists and thus whether it is a good model to use a uniform deposition velocity for a given particle size.

For the 0.5 μm particles Figure 2.6 shows a linear relation ($r=0.99$) with the intercept being close to zero. The slope of a regression line represents the deposition velocity. This slope obtained is $0.00016 \pm 0.00002 \text{ m s}^{-1}$.

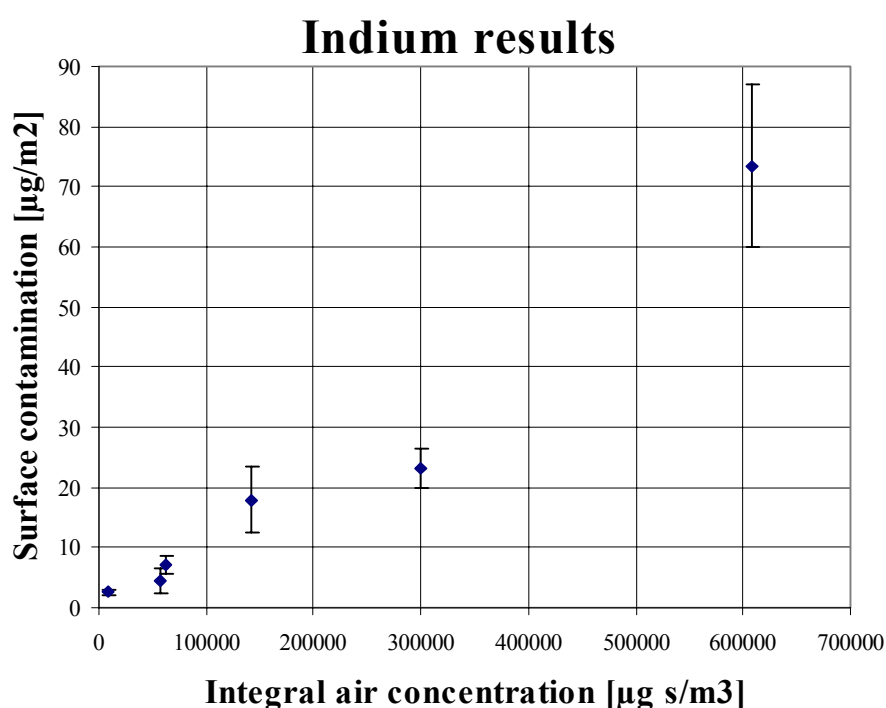


Figure 2.6 Surface contamination plotted versus the integrated air concentration in 6 different tests. The error bars show the standard deviation on the mean for each test.

For the 2.5 μm particles a less ideal result is seen in Figure 2.7. Here, a regression has a lower correlation factor ($r=0.84$) and the intercept is different from zero suggesting that there is a background on the skin wipes. However, a intercept of zero still lies within the 95% confidence interval. Since sampling from unexposed persons has not shown any tracer background, it is likely that the results shown in Figure 2.7 is an indication of the natural variability of the deposition velocity. It should be noted whereas for the 0.5 μm particles, a variation in integrated air concentration over almost two orders of magnitude were obtained, only a variation of 3 was achieved for the 2.5 micron particles.

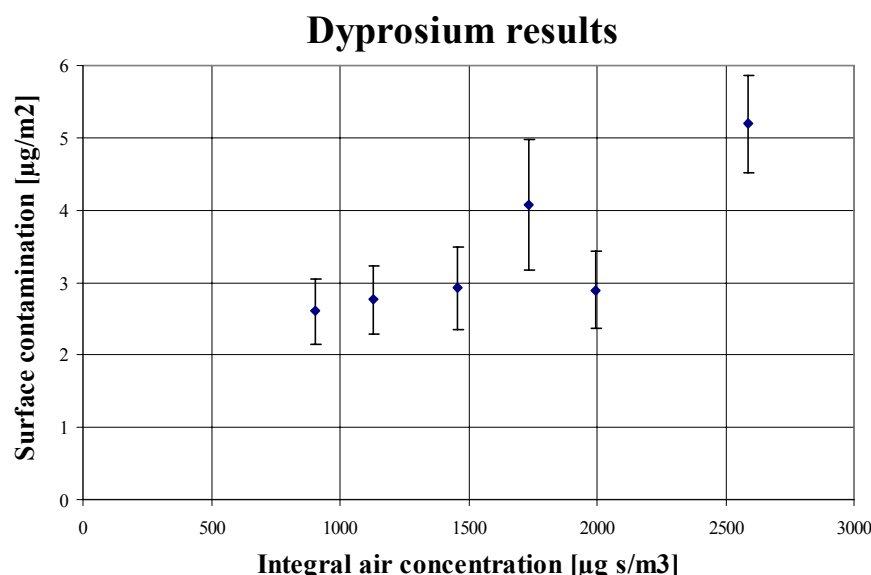


Figure 2.7 Surface contamination plotted versus the integral air concentration in 7 different tests with $2.5 \mu\text{m}$ particles. The error bars shows the standard deviation on the mean for each test.

In summary, the results obtained in realistic indoor environments was in good agreement with the test chamber results. In general the deposition velocity increased with increasing particle size. For the $2.5 \mu\text{m}$ particles the deposition velocity was 25 to 50 % higher in the test chamber than in the realistic environments, but this can be attributed to the variability due to different tests persons being exposed and the different air flow patterns in the two environments.

Factors relevant to the outdoor environment

Although the human population spends the majority of its time indoors, it is obviously also important, in the event of a nuclear accident, to assess the risk, from dermally deposited particulates, to those engaged in outdoor activities. Wind tunnels are commonly used to carry out controlled experiments under simulated outdoor conditions, and other workers (e.g. Gudmundson *et al.*, 1992) have carried out aerosol deposition measurements on human phantoms under elevated air velocity conditions. However, no experiments have yet been carried out using anthropomorphic bodies which are heated to human body temperature. In the present work, it was intended that measurements of tracer aerosol deposition velocities would be made to the surface of the heated cylinder which had been used in the test chamber experiments described earlier. However, the wind tunnel available was of the non-recirculating type and it was anticipated that it would require an experimental duration of several hours before an appreciable quantity of tracer aerosol sweeping past a body would be deposited at a detectable level. The use of the labelled silica particles employed in the indoor experiments was considered prohibitively expensive for the wind tunnel tests and a more economical alternative is described below.

An aerosol generator developed for the study of aerosol deposition onto forest canopies, as described by Kinnersley (1997), was used for the wind tunnel deposition experiments. Uranium aerosol is generated as follows: nine side-stream nebulisers connected to a clean air supply deliver nebulised uranyl acetate (depleted) from an aqueous solution to a conical expansion chamber, where the nebulised aerosol particles are mixed with diluting air. The aerosol then

passes a radioactive charge neutralising source (74 MBq ^{85}Kr) and enters a furnace, where residual water is removed from the particles. A delivery tube connects the generator to the wind tunnel.

Using the system described above, uranyl acetate aerosol particles with an aerodynamic diameter of $1.0\ \mu\text{m}$ and a geometric standard deviation (σ_g) of 1.26 were generated. Wind tunnel experiments were then carried out, at wind-speeds of $2\ \text{m s}^{-1}$ and $4\ \text{m s}^{-1}$, to determine the deposition velocity of those particles to felt surfaces attached to the surface of the aluminium cylinder which was used in the test chamber experiments. The cylinder was heated to body temperature.

The technique chosen to analyse the felt surfaces for deposited aerosol was Delayed Neutron Counting (DNC). DNC makes use of the fact that a fissile element (such as ^{235}U or ^{239}Pu) may undergo fission when bombarded by a neutron flux, producing unstable isotopes which may decay by the emission of a beta-particle to form an unstable species which is neutron rich. This unstable nucleus may then decay by the emission of a neutron (Benzing *et al.*, 1993); the half-life of the second emission is extremely short ($T_{1/2} \sim 10^{-20}\text{s}$) which makes it seem that the half-life of the neutron decay is the same as the beta decay. The beta decay processes have half-lives ranging from a fraction of a second to approximately 1 minute.

The samples were irradiated in a neutron flux of $1 \times 10^{12}\ \text{n cm}^{-2}\ \text{s}^{-1}$ and delivered by an automated system to an array of nine BF_3 detectors. The quantity of uranyl acetate present in the samples was deduced by comparing the neutron spectrum with that of the reference standard which contains 100 mg of uranium nitrate.

To date, far one successful experiment has been carried out in the wind tunnel and the result is presented in Table 2.10. This first experiment indicates a significant increase in deposition velocity with increasing wind speed as should be expected for particles that are susceptible to inertia effects. This can be compared to the measured deposition velocity on the cylinder under the low air velocity conditions in the test chamber ($0.25\ \text{m s}^{-1}$), where a deposition velocity of $3.3 \times 10^{-4}\ \text{m s}^{-1}$ was found for $2.5\ \mu\text{m}$ particles.

Table 2.10 shows the aerosol deposition velocities measured on the cylinder surfaces in the wind tunnel.

	Wind speed [m s^{-1}]	
	2	4
Deposition velocity [$10^{-4}\ \text{m s}^{-1}$]	30	48
s.d. [%]	10	10

2.4 Doses received from contamination of skin

The parameters obtained from the experimental work in this study have been used to model the dose from deposits on skin, clothing and hair after an accidental release of radionuclides. An estimation was made of the relative contribution to dose from skin contamination in a dry deposition scenario following an airborne release of radioactive matter. Both the skin dose from β - and γ -emitters and the whole body dose from γ -emitters have been considered.

To facilitate a comparison with the doses received from radioactive matter deposited on other surfaces in the environment after an accidental release, the skin-related doses were calculated on the basis of near-surface air concentrations of different contaminants measured after the Chernobyl accident. These

concentrations were derived from measurements made in the Novozybkov area of Russia over the first two months after the release (Kryshev, 1996). The time-integrated air-concentrations of measurable particles are shown in Table 2.11.

The above reference does not distinguish between the different chemical forms of iodine. However, the COSYMA model suggests that 99% of the iodine is in the elemental form (with a dry deposition velocity of 0.01 m s^{-1}), while the remaining 1% is in organic form (deposition velocity: $5 \times 10^{-4} \text{ m s}^{-1}$) and this partitioning has been assumed in the present work.

It should be considered that the concentration of aerosol in the Novozybkov area was greatly depleted by rain, which lead to high ground contamination levels. However, it followed from the air concentrations and from measured deposition velocities to a lawn (Roed, 1990) that the contribution to the ground contamination level from dry deposition of ^{137}Cs in the area (the nuclide which essentially determines the long-term doses from the ground) was only about 8 kBq/m^2 .

With the exception of iodine, for which the chemistry is more complex, the different contaminant aerosol was divided into two groups : the volatile group (^{132}Te , ^{134}Cs , ^{137}Cs , ^{99}Mo , ^{103}Ru and ^{106}Ru) with lower Activity Median Aerodynamic Diameter, AMAD, values of the order of $0.7 \mu\text{m}$ and the refractory group with higher AMAD values of the order of $4 \mu\text{m}$, to which ^{140}Ba , ^{95}Zr , ^{141}Ce , ^{144}Ce , ^{89}Sr and ^{90}Sr belong (Reineking *et al.*, 1987; Rulik *et al.*, 1989; Dorrian, 1997).

As indicated above, the dry deposition velocities of the different contaminant aerosol to a grassed lawn were estimated from field measurements made shortly after the Chernobyl accident (Roed, 1990) and from COSYMA parameters. The estimates of dry deposition velocities to skin were based on the results obtained in the current project.

It was assumed in the calculations that the people in the area stayed indoor during virtually the entire deposition phase. The relationship between the indoor and outdoor air concentrations was found from the following expression:

$$C_i / C_o = f \lambda_r / (\lambda_r + \lambda_d)$$

(Roed & Cannell, 1987), where λ_r is the fraction of air exchanged per unit of time, λ_d is the fraction of aerosols indoors depositing per unit of time and f is the filtering factor (the fraction of aerosols in air entering the building which is not retained in cracks and fissures of the building structure).

Numerous experiments carried out under a previous project (Fogh *et al.*, 1997) have shown that the filtering factor can be assumed to be 1 and that a realistic value of λ_r is 0.4 h^{-1} for western European houses of good construction. Further, it was estimated from the experimental data that λ_d would be in the order of 3 h^{-1} for aerosols of the refractory group and 0.4 h^{-1} for most of the volatiles, with the exception of the rutheniums, for which λ_d was estimated to be 1.1 h^{-1} and of iodine, for which the λ_d estimate was based on the publications of Kocher (1980) and Roed & Cannell (1987). The corresponding C_i / C_o relationships can be seen in Table 2.11. The total integrated skin deposition (kBq/m^2) was calculated by multiplication of the time-integrated air concentrations by the indoor/outdoor relationship and the skin deposition velocities. These values are also listed in Table 2.11.

A 'half-life correction' was then introduced, taking into account both the radioactive decay half-lives of the isotopes and a 'clearance' half life, by which the skin contaminant concentration is depleted. The COSYMA modellers assume the latter to generally be of the order of 30 days, and this value was applied in the calculations.

For estimation of the dose contribution to the body from gamma emission on skin, Monte Carlo calculations were performed using the MCNP code. A simplified model was applied, in which a tissue equivalent ICRP sphere was irradiated by a surface contamination of variable energy. It was found that the sensitivity of this model towards changes in sphere diameter was low. In the model the sphere was placed at a height of 1m above ground. Figure 2.8 shows the energy dependence of the gamma doses received per gamma ray emitted each second from an area of 1 cm². The relative uncertainty on the Monte Carlo calculations expressed by Figure 2.8 was in all cases less than 1%.

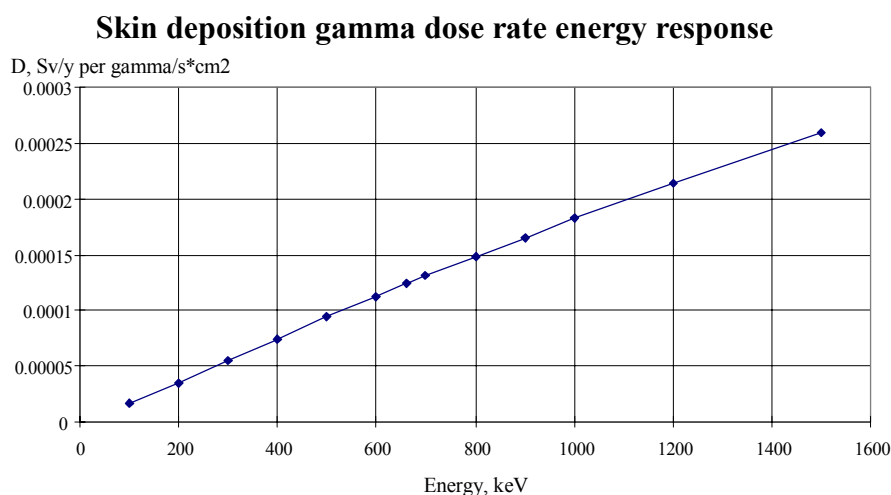


Figure 2.8 Monte Carlo modelled whole-body gamma doses received from skin contamination. Dose responses as a function of gamma ray energy.

Another dose contribution from contamination deposited on skin results from beta radiation. The calculations of this contribution required a knowledge of the dose rate to the basal layer of the epidermis for the different isotopes. Nuclide-specific absorbed dose rates at an epidermis equivalent depth in water (ca. 70 µm) from various beta sources were derived from the figures stated in ICRU report 56 (1997). The ICRU figures were mostly based on the Monte Carlo calculations of Cross et al. (1992). The results are shown in Table 2.12. These dose rate factors were found to be in fairly good agreement with the corresponding factors reported by Faw (1992).

By multiplication of the skin contamination levels by the 'half-life correction factor' and the dose rate factors for beta exposure at a depth of 70 µm, the total doses to the skin were found. Also presented in Table 2.12 are the doses weighted by a factor of 0.01 * 0.15, corresponding to respectively the tissue weighting factor for skin (according to ICRP 60, 1990) and the fraction of the total skin constituted by the hands and the head (according to the report of the task group on reference man (ICRP 23, 1974)). For simplicity, hair has not been considered in these calculations, which according to the deposition velocities recorded in the project together with the extra distance and shielding provided by the hair, would make the estimates conservative.

The calculations of Rohloff and Heinzelmann (1996) clearly demonstrate that the dose rates received by photon radiation to the basal layer of the skin epidermis are negligible compared with the contributions from beta radiation.

Table 2.11 Parameters applied in the calculations of doses received from gamma emission from skin contamination. Values relating to published air concentrations of different isotopes measured in near-ground level air in Novozybkov (Kryshev, 1996). Integrated air concentrations are given together with radioactive half-lives, AMADs, indoor/outdoor air concentrations, deposition velocities to skin and grassed lawn, half-life correction factor (over 1 year), doses per Bq/cm² (by Monte Carlo) and total doses received by this pathway.

Isotope	Integr. air contam. B (Kryshev) [Bq s m ⁻³]	T _{1/2} [days]	AMA D [μm]	Ci/Co []	V _d , face/ hand [m s ⁻¹]	v _d grass [m s ⁻¹]	Contam on skin [Bq m ⁻²]	Half-life correct. []	Dose [Sv per Bq cm ⁻²]	Total dose [Sv]
I-131 (organic)	1.79E+06	8	0.5	0.36	0.005	5.00E-04	3222	0.0249	6.80E-05	5.47E-07
Te-132	1.81E+07	3.25	0.7	0.5	0.001	4.30E-04	9050	0.0115	3.50E-05	3.67E-07
Cs-134	8.93E+06	767	0.7	0.5	0.001	4.30E-04	4465	0.1140	2.27E-04	1.16E-05
Cs-137	1.78E+07	10986.5	0.7	0.5	0.001	4.30E-04	8900	0.1182	1.02E-04	1.07E-05
Ba-140	1.08E+07	12.8	4	0.12	0.012	7.50E-04	15552	0.0354	2.35E-05	1.3E-06
Zr-95	2.67E+06	65.5	4	0.12	0.012	7.50E-04	3844.8	0.0813	1.36E-04	4.25E-06
Mo-99	5.18E+06	2.75	0.7	0.5	0.001	4.30E-04	2590	0.0099	2.66E-05	6.86E-08
Ru-103	9.10E+06	39.6	0.7	0.27	0.001	4.10E-04	2457	0.0674	8.70E-05	1.44E-06
Ru-106	2.28E+06	369	0.7	0.27	0.001	4.10E-04	615.6	0.1096	3.20E-05	2.16E-07
Ce-141	3.17E+06	32.5	4	0.12	0.012	7.50E-04	4564.8	0.0616	1.10E-05	3.1E-07
Ce-144	2.14E+06	284.4	4	0.12	0.012	7.50E-04	3081.6	0.1072	3.20E-06	1.06E-07
Sr-89	1.32E+05	50.5	4	0.12	0.012	7.50E-04	190.08	0.0743	0	0
Sr-90	1.41E+04	10585	4	0.12	0.012	7.50E-04	20.304	0.1182	0	0
Np-239	1.68E+07	2.4	4	0.12	0.012	7.50E-04	24192	0.0087	1.20E-05	2.55E-07
I-131 (elem.)	1.77E+08	8		0.07	0.010	1.00E-02	123900	0.0249	6.80E-05	2.1E-05

Table 2.12 Factors applied in the calculation of the beta doses to skin contaminated by indoor deposition of airborne radiopollutants with the air concentrations measured by Kryshev (1996) in the Novozybkov area following the Chernobyl accident.

Isotope	Integr. air contam. B (Kryshev) [Bq s m ⁻³]	T _{1/2} [days]	AMAD [μm]	Ci/Co []	v _d , face/ hand [m s ⁻¹]	Skin contam [Bq m ⁻²]	Dose rate at 70 μm (ICRU56) [Sv y ⁻¹ per Bq cm ⁻²]	Half-life correct. []	Total skin dose [Sv]	Dose total tissue/% weighted [Sv]
I-131 or	1.79E+06	8	0.5	0.36	5.00E-03	3222	0.012	0.0249	9.65E-05	1.45E-07
Te-132	1.81E+07	3.25	0.7	0.5	1.00E-03	9050	0.0079	0.0115	8.29E-05	1.24E-07
Cs-134	8.93E+06	767	0.7	0.5	1.00E-03	4465	0.0094	0.1140	0.000479	7.18E-07
Cs-137	1.78E+07	10986.5	0.7	0.5	1.00E-03	8900	0.014	0.1182	0.001473	2.21E-06
Ba-140	1.08E+07	12.8	4	0.12	1.20E-02	15552	0.013	0.0354	0.000717	1.08E-06
Zr-95	2.67E+06	65.5	4	0.12	1.20E-02	3844.8	0.01	0.0813	0.000313	4.69E-07
Mo-99	5.18E+06	2.75	0.7	0.5	1.00E-03	2590	0.013	0.0099	3.35E-05	5.03E-08
Ru-103	9.10E+06	39.6	0.7	0.27	1.00E-03	2457	0.0054	0.0674	8.95E-05	1.34E-07
Ru-106	2.28E+06	369	0.7	0.27	1.00E-03	615.6	0.016	0.1096	0.000108	1.62E-07
Ce-141	3.17E+06	32.5	4	0.12	1.20E-02	4564.8	0.014	0.0616	0.000394	5.91E-07
Ce-144	2.14E+06	284.4	4	0.12	1.20E-02	3081.6	0.0079	0.1072	0.000261	3.92E-07
Sr-89	1.32E+05	50.5	4	0.12	1.20E-02	190.08	0.015	0.0743	2.12E-05	3.18E-08
Sr-90	1.41E+04	10585	4	0.12	1.20E-02	20.304	0.013	0.1182	3.12E-06	4.68E-09
Np-239	1.68E+07	2.4	4	0.12	1.20E-02	24192	0.015	0.0087	0.000319	4.78E-07
I-131 el.	1.77E+08	8		0.07	1.00E-02	123900	0.012	0.0249	0.003712	5.57E-06

On the parts of the body that are covered by clothes, the beta skin doses are much lower due to the shielding effect of the clothing. The Tables in Appendix A of the ICRU 56 report show that due to the similar beta attenuation characteristics, it is reasonable to assume that equal mass-thickness' of clothing and tissue are equivalent in dose considerations. From the dose rate factors given in ICRU 56 it followed that practically no beta doses would be received through 3 mm thick clothing. The numbers presented in Table 2.13 express the doses that would be received through 0.4 mm thick clothing.

The dose rate factors found for 0.4 mm clothing were in reasonable agreement with those reported by Taylor et al. (1997) for a 26 mg cm⁻² thick layer of cotton with a density of 0.7 g cm⁻³. Taylor et al. also demonstrated that an air gap of 1 cm between the skin and the clothing could halve the doses received from beta radiation with higher energies (above 0.4 MeV).

Also for the clothing, the clearance half-life recommended by the COSYMA modellers was applied. The deposition velocities to clothing were evaluated from results of the current project and from results reported by Lange (1995). As before, both the total doses to the skin epidermis and the weighted dose (by tissue weight factor and percentage of skin covered) are shown in Table 2.13.

Table 2.13. Factors applied in the calculation of the beta doses to skin, through contamination on clothing by indoor deposition of airborne radiopolutants with the air concentrations measured by Kryshev (1996) in the Novozybkov area following the Chernobyl accident.

Isotope	Integr. air contam. (Kryshev)	T _{1/2}	AMAD	Ci/Co	v clothing	Contam cloth.	Half- life correct.	Dose rate at 0.4 mm (ICRU56)	Total dose	Dose total tissue/% weighted
	[Bq s m ⁻³]	[days]	[µm]	[]	[m s ⁻¹]	[Bq m ⁻²]	[]	[Sv y ⁻¹ per Bq cm ⁻²]	[Sv]	[Sv]
I-131 or	1.79E+06	8	0.5	0.36	1.00E-03	644	0.0249	0.002637	4.24E-06	3.39E-08
Te-132	1.81E+07	3.25	0.7	0.5	1.70E-03	15385	0.0115	5.782E-5	1.03E-06	8.25E-09
Cs-134	8.93E+06	767	0.7	0.5	1.70E-03	7591	0.1140	0.002278	0.000197	1.58E-06
Cs-137	1.78E+07	10986.5	0.7	0.5	1.70E-03	15130	0.1182	0.003373	0.000603	4.83E-06
Ba-140	1.08E+07	12.8	4	0.12	2.70E-03	3499	0.0354	0.004284	5.32E-05	4.25E-07
Zr-95	2.67E+06	65.5	4	0.12	2.70E-03	865	0.0813	0.000752	5.29E-06	4.24E-08
Mo-99	5.18E+06	2.75	0.7	0.5	1.70E-03	4403	0.0099	0.005895	2.58E-05	2.07E-07
Ru-103	9.10E+06	39.6	0.7	0.27	1.70E-03	4177	0.0674	0.000243	6.84E-06	5.47E-08
Ru-106	2.28E+06	369	0.7	0.27	1.70E-03	1047	0.1096	0.010827	0.000124	9.94E-07
Ce-141	3.17E+06	32.5	4	0.12	2.70E-03	1027	0.0616	0.00148	9.38E-06	7.50E-08
Ce-144	2.14E+06	284.4	4	0.12	2.70E-03	693	0.1072	0.000251	1.86E-06	1.49E-08
Sr-89	1.32E+05	50.5	4	0.12	2.70E-03	42.8	0.0743	0.00784	2.49E-06	2.00E-08
Sr-90	1.41E+04	10585	4	0.12	2.70E-03	4.57	0.1182	0.002917	1.58E-07	1.26E-9
Np-239	1.68E+07	2.4	4	0.12	2.70E-03	5443	0.0087	~0	-	-
I-131 el.	1.77E+08	8		0.07	1.00E-02	123900	0.0249	0.002637	0.000816	6.52E-06

Conclusions

From Table 2.11 it can be seen that with the air concentrations measured at Novozybkov, the total dose contribution received over a few months from gamma radiation from skin contamination amounts to about 52 µSv. This can be compared with the external dose contribution from contamination on other surfaces in the environment (e.g., soil, roofs, walls of buildings and pavings), which, with a total deposition of only 8 kBq/m², as was assumed in these calculations,

would be of the order of 10-50 μSv over the first year, depending on the degree of shielding provided by the dwellings (Andersson, 1996). Dry deposition after the Chernobyl accident actually led to contamination of living areas in Russia with levels which were several hundred times higher. Here the skin contamination would give a gamma dose of several mSv.

It follows from Table 2.12 that the dose from the beta radiation to the epidermal layer of the directly exposed skin is about 8 mSv, in total. With a contamination level several hundred times greater, the skin dose would be several Sv. According to ICRP publication 59 (1991) the threshold for acute radiation effects by exposure of large areas of skin is generally assumed to be about 20 Sv, although acute tissue breakdown has been reported for doses as low as 15 Sv. These doses should also be compared with the risk of skin cancer mortality, which is estimated to be $2 \cdot 10^{-4} \text{ Sv}^{-1}$, and with the skin morbidity risk ($9.8 \cdot 10^{-2} \text{ Sv}^{-1}$), which is extremely high at doses of the range of a Sievert (ICRP 59, 1991).

The doses in the last column of Table 2.12 (total over isotopes = $12.2 \mu\text{Sv}$), which were weighted with the skin tissue weight factor and the percentage of the body not covered by clothes, make it possible to evaluate the effect of the skin irradiation relative to that from irradiation of other organs. However, this weighting may result in an under-estimation of the skin cancer risks. ICRP 59 states that the stochastic risks are dependent on the exposure of the area to sunlight (UVR). An exposure of all the skin that is normally exposed to UVR is said to give a risk comparable to that for whole-body exposure.

The doses received through a layer of clothing of 0.4 mm in thickness were in the Novozybkov case study found to amount to a total of about 2 mSv. In other words, the thin layer of cotton locally reduces the beta skin dose by a factor of about 4. As mentioned above this factor may be greater due to the air gap between the contaminated clothing and the skin.

As can be seen from the tables, in the Novozybkov example ^{131}I has the highest relative importance in connection with all dose contributions related to skin contamination. This is due to the large amount released, the high deposition velocity to skin and the short skin clearance half-life, which make the radiological half-lives somewhat less important. For all skin contamination dose pathways in the Novozybkov case, the caesiums (^{137}Cs and ^{134}Cs) give the second largest contribution.

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3 Summary of main achievements

The main achievement of work package 1 is the design and validation of the sampling protocol for particles on skin. This protocol is the basis for the retention and clearance experiments in work package one and the deposition experiments in work package 3. The protocol will also be useful in other fields of science, e.g. skin exposure assessments in occupational hygiene.

In the validation experiments in work package 1, human skin was used to investigate whether the wiping gave consistent results and rat skin was used to measure the actual wiping efficiencies. It was also established that using different wiping areas gave similar surface concentration results.

A fluorescence scanning system was developed and fluorescence microscopy was used to provide additional information on the impact of sampling on the distribution of deposited aerosol particles.

Clearance experiments carried out with the fluorescence scanning system suggested a clearance half life of particles from skin, which was lower than that generally accepted and more research is needed here.

Sampling protocols for clothing and hair were established and used to determine deposition velocities. More work is needed in order to determine the depth distribution of particles in hair, as well as the difference between synthetic and natural fibres.

Deposition to hair has been measured using wigs, obtaining deposition velocities close to those for skin for the supra micron particles, but significantly higher for the sub-micron particles.

Forced clearance by washing in domestic washing machines has been measured for different fabrics and removal efficiencies from 20 to 89 % were found.

In work package 3, deposition velocities have been measured for three particle sizes in a test chamber and two particle sizes in realistic indoor environments. The effect of electrical grounding and heat generated turbulence on deposition has been examined. Deposition velocities on a heated cylinder and from human body surfaces have been compared. Overall, a coherent dataset on skin deposition velocities has been compiled.

A wind tunnel has been used to simulate outdoor conditions, but only one experiment has yet been performed. This experiment showed a clear increase in deposition velocity with increasing wind speed, but more work is clearly merited.

In Figure 3.1 the different deposition velocities obtained in various test environments have been presented together. Looking at the ‘normal’ condition test chamber experiments and the realistic indoor environments it seems that there is a linear increase in deposition velocity with particle size. The grounding of the arm was seen to reduce deposition somewhat. For outdoor conditions there is a significant increase in deposition by almost an order of magnitude compared to the expected value for 1 μm particles.

Summary of results

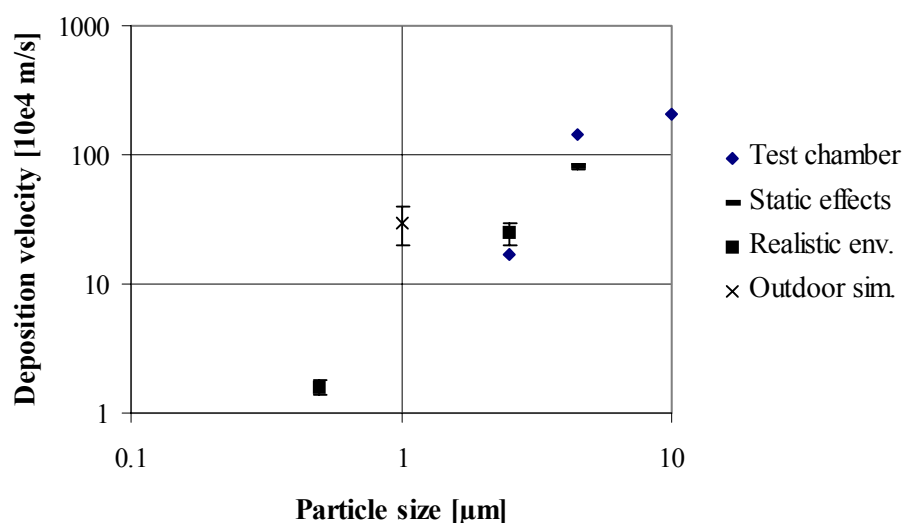


Figure 3.1 Review of deposition results to skin under different conditions.

A model was established for the calculation of doses received from contamination of the human body after an airborne release of radioactive matter. To investigate the relative importance of different isotopes that may deposit following an accident, measured air concentrations of different isotopes in near-ground level air in Novozybkov, Russia after the Chernobyl accident were applied. By multiplication of these time-integrated air concentrations by the relationship between the indoor and outdoor air concentrations, which has been established experimentally for different groups of aerosol, the indoor air concentrations were found. These were, in turn, multiplied by measured aerosol-specific deposition velocities to find the total amounts deposited to an area of skin or clothing. In the dose calculations, natural decay and clearance were taken into account. Doses from gamma emission from the contaminants were calculated on the basis of a simple Monte Carlo model, in which an ICRU sphere was irradiated from the surface. The beta doses to the skin were calculated from published data for an epidermis equivalent depth in water and at a depth corresponding to 0.4 mm thick cotton clothing. It was found that the largest contribution to both gamma and beta doses came from ^{131}I , and the second-largest from ^{134}Cs and ^{137}Cs . The gamma doses were found to be in the same range as those received over the first year from contamination of outdoor surfaces. A significance of skin doses from beta emission was also detected. In areas which were highly contaminated by dry deposition after the Chernobyl accident, skin cancer is estimated to have had a rather high probability.

4 Research to be performed in the last year

The model developed for calculation of doses received from an airborne contamination of human body surfaces has indicated that both beta and gamma radiation may in this context be significant. However, a crucial parameter, which requires a more detailed determination, is the clearance rate, by which the concentrations of radioactive substances are normally depleted on skin and clothing as well as on hair.

The primary effort remaining within work package 1 will be focused on studies of clearance rates of particles from skin. Here, both the developed fluorescence scanning system and the protocol for skin wiping will be used to follow a skin contamination on a number of test persons. Also the effect of various decontamination procedures, such as hand washing, will be examined.

Finally the methods developed and applied in work packages 1 will be to study contact transfer, that is, the contamination of skin when touching other contaminated surfaces. Here data is needed in order to judge the order of magnitude of the dose contribution from this pathway.

Two of the tasks examined so far in work package 2 will be further investigated in the last year: deposition to hair and clearance from clothing. In particular, the effect of fabric type will be examined (synthetic contra cotton, etc.), the long term clearance of the particles during natural wear of clothing and the long term clearance of particles from hair.

For the last year two more tasks have been scheduled: "clearance from hair" and "depth distribution of deposits in clothing". Both these parameters will have implication for modelling of the dose. Experiments where the clearance from human hair is followed over an extended period of time (1 - 2 months being the likely time range) will be performed.

The deposition velocity to skin have already been thoroughly examined, but some extra results will be obtained in the last year as a part of experiments where test persons are exposed in studies aimed at measuring clearance rates. More work with factors relevant to the outdoor environment is also needed as only one experiment has been made in the wind tunnel to date.

In the modelling of the dosimetric effects of deposition to the human body surfaces a continued effort will be made to incorporate the experimental results obtained in the model.

The clearance rate of particles from the skin is one of the parameters that has been shown to be of great importance. In the calculations that have been made so far, the estimation of this parameter has relied entirely on the value applied by the COSYMA code modellers (i.e. a clearance half-life of 30 days). However, it is evident that clearance half-lives will be different for different surfaces and aerosol sizes. Preliminary work in this project has indicated that clearance half-lives may be considerably shorter than the COSYMA value.

In addition to clearance rate, other model values will be verified/improved during the next project period. Currently, the model is linked to a case study of doses received in Novozybkov. To make the model applicable in a wider sense and eliminate the complexity of the radionuclide dispersion processes, doses will in future work be expressed relative to a more easily measurable quantity, such as the deposition to a grassed lawn. So far, the model has, for simplicity, only described a hairless target person. However, much of the data required to

take into account the special deposition conditions to hair as well as the beta dosimetric implications has been generated in the project, and the influence of hair will be investigated during the next project period.

5 Publications achieved

The publications achieved so far mostly includes conferences proceedings, etc. The partners are planning for three journal paper dealing with the sampling of particles from skin issue, the measured deposition velocities and the dosimetric implications of the obtained parameters.

Byrne, M.A.; Goddard, A.J.H.; Lockwood, F.C. and M. Nasrullah, Aerosol deposition on internal buildings surfaces: comparison of modelling and measurement. Proceedings of the 10th Annual conference of the Aerosol Society, pp.75-80, 1996.

Byrne, M.A.; Goddard, A.J.H.; Lockwood, F.C. and M. Nasrullah, Aerosol deposition on internal building surfaces: experimental validation of a computational model. Proceedings of RoomVent '96, Japan, pp 105-112, 1996.

Byrne, M.A.; Goddard, A.J.H.; Lockwood, F.C. and M. Nasrullah, Particulate pollution interactions with indoor surfaces: measurements and modelling for risk assessment and contaminant control . Proceedings of the 17th Air Infiltration and Ventilation Centre Conference, Sweden, Vol. 1 pp 65-74, 1996.

Goddard, A.J.H.; Byrne, M.A.; Lange, C.; Roed, J. and Lai, C.K., Tracer-labelled Aerosol Deposition Measurements on Internal Building Surfaces: Implications for Indoor Air Quality. 6th International conference on Indoor Air Quality and Climate, Vol. 3, pp 839-845, 1996.

Fogh, C.L.; Byrne, M.A.; Roed, J. and A.J.H. Goddard, Size Specific Indoor Aerosol Deposition Measurements and Derived I/O Concentration Ratios. Atmospheric Environment, Vol. 31, No. 15, pp. 2193-2203, 1997.

Vollmair, D.V., Byrne, M.A., Hotchkiss, S.A.M. and A.J.H. Goddard, An Experimental Study of the Dermal Penetration of Aerosol Particles. Proceedings of the 11th Annual Conference of The Aerosol Society of the British Isles, pp.91-96, 1997.

6 Executive summary

It has long been recognised that a relationship exists between the occurrence of some adverse health effects and the dermal deposition of airborne contaminants. In the radiological context, this contribution has, to date, been largely ignored in estimates of the total dose to exposed individuals, but Jones has shown (Jones 1990, EUR 13013) that the predicted number of early deaths arising due to gamma and beta radiation doses is sensitive to the value used for aerosol deposition and residence time on skin. However, reliable aerosol depo-

sition and clearance data for skin, hair and clothing are currently extremely limited. The present work aims to redress this by using sensitive tracer aerosol generation and detection techniques (employing both neutron activatable and fluorescent tracers) to study the deposition of airborne particles to skin, hair and clothing, and to investigate the retention and clearance of the deposited matter. The ultimate objective of the work is to develop dosimetric models which can use the experimental data as input.

An accurate estimation of the deposition velocity to skin - that is, the aerosol flux to the skin, divided by the ambient aerosol concentration- is underpinned by the ability to precisely measure the aerosol mass deposited on the body surface. In the present work, a variety of dermal exposure assessment techniques commonly used in the occupational environment were tested for suitability as tracer particle sampling technique, both in-vivo and in-vitro. Tests were carried out using neutron activatable and fluorescent particles (in the size range 0.5 microns to 8 microns) on in-vivo human skin and in-vitro rat skin. Qualitatively, skin wiping was found to be a satisfactory sampling technique for tracer aerosol particles, with good reproducibility and high integrity, borne out by the strong correlation between recovered tracer mass and wiped area. Quantitatively, wiping was found to remove of the order of 70% of the tracer aerosol from the skin.

Wiping, and other particle removal techniques, were also assessed in this work from the point of view of dermal decontamination efficacy, following an accidental radioactive aerosol exposure. Due to its high particle removal efficiency, wiping (and also tape-stripping) was considered to have some value as a dermal decontamination technique. However, analysis of repeated wipes on the same area of skin indicated that there exists a dislodgeable particle fraction. Furthermore, in-vitro experiments, where skin was exposed to fluorescent particles, wiped and then analysed by fluorescent microscopy, provides evidence of redistribution of particles following wiping.

In addition to dedicated skin decontamination strategies which might be implemented following an accidental aerosol exposure, a fluorescence scanning system was developed so that the time course of decontamination on the skin during normal activities - everyday washing, or simple wearing-could be determined. Limited experiments with the scanning system indicated that cold water washing removed a substantial proportion of deposited 4.5 μ m particles. Human activity experiments, whereby exposed individuals engaged in normal indoor and outdoor walking, yielded a clearance half life for these particles of the order of a few hours, significantly shorter than the value used in accident consequence codes such as COSYMA. Bearing in mind that the in-vitro experiments show that the penetration of particles into skin is strongly dependent on residence time (and on particle size) and that modelling indicates that skin clearance half life is an important determinant of dose, more experimental work to determine skin clearance half-lives is planned. These measurements will address particle clearance from skin during washing, and also through normal wearing.

It is considered that a significant amount of information has already been generated from the experimental work on skin sampling carried out under the contract, which not only has importance in the radiological context following an accident, but also in the occupational health context. A dermal exposure pathway which is relevant to both contexts is that of contact transfer between the skin and contaminated indoor surfaces, and it is planned that experiments to assess the significance of this pathway shall be carried out during the remainder of the contract.

Having developed a skin sampling protocol as outlined above, aerosol deposition velocity measurements on skin could be made, by exposing human vol-

unteers to tracer aerosol in test chambers and in test rooms. The results indicated that the deposition velocities were in the range $0.4 \times 10^{-4} \text{ ms}^{-1}$ - $219 \times 10^{-4} \text{ ms}^{-1}$, for particles in the size range 0.5 microns - 8 microns. These values were at least an order of magnitude higher than deposition velocities measured to inert building surfaces, both during the present measurements and as part of previous research, and for this reason, efforts were made to understand the underlying physics of aerosol interaction with the human body. The influence of the body's electrostatic potential on aerosol deposition was demonstrated by attaching an electrical grounding strap to one arm of a volunteer; this had the effect of reducing the deposition velocity of 4.5 μm particles by a factor of two. Air velocities measured in close proximity to the volunteer were found to be higher than ambient, suggesting that air turbulence, which promotes aerosol impaction, may arise due to the body's heat island. Measured aerosol deposition velocities on test surfaces attached to a volunteer and to a heated aluminium phantom indicated that surface roughness and electrostatic charge influenced aerosol deposition in the particle size range studied. Preliminary experiments at elevated air velocities (2 ms^{-1} and 4 ms^{-1}) were carried out in a wind tunnel to measure aerosol deposition rates of 1 micron particles on the heated cylinder; these measurements indicated that aerosol deposition on the body in the outdoor environment might be considerable, and further measurements to elucidate this aspect are planned during the remainder of the contract period.

It is envisaged that the database of aerosol deposition velocities to skin, which is already extensive, will be added to in the remaining contractual period, since some of the planned aerosol retention studies on hair and clothing will necessitate further exposure of skin, which can then be sampled by wiping.

In an accident situation, in addition to aerosol deposition and clearance data for skin, doses also arise from aerosol interaction with hair and clothing. Due to the versatility of neutron activation analysis, sampling protocols for hair and clothing are relatively straightforward, since these materials, after an aerosol deposition interval, can be destructively analysed. Experiments were carried out to determine aerosol deposition velocities to hair and clothing, using both synthetic wigs and real human hair, and a range of synthetic and mixed-fibre clothing. Measured deposition velocities were found to be comparable to those measured for skin, although somewhat higher for 0.5 micron particles on hair. Limited clothing washing experiments indicated a dependence of particle removal efficiency on particle size. Also, the data suggest that the micro-physical fibre structure (smooth in the case of synthetic fibres and rougher in the case of natural fibres) of clothing was a more important determinant of particle removal efficiency than the macro-physical weave of the garment itself. Further measurements are planned during the remainder of the contract period to elucidate this finding. Further work is also planned to determine clearance half-lives of particles from hair and clothing under normal human activity (i.e. wearing, but no washing, in the case of clothing, and washing in the case of hair). In addition, it is planned that data are generated to permit estimates of the dose to skin arising from radioactive aerosol deposition on clothing, by making measurements of depth profiles of particle deposits in clothing.

To complement the experimental work, a computational model was developed for the calculation of doses from contamination of the human body after an airborne release of radioactive matter. Using measured aerosol concentrations for different isotopes in near-ground level air in Novozybkov, Russia, after the Chernobyl accident, size-specific indoor air concentrations were deduced using an empirical formula derived under a previous research contract. These were then multiplied by experimentally-determined aerosol deposition velocities to skin to determine the total amount of radioisotope deposited on an area of hair and clothing. Dose calculations were made on the basis of a simple

Monte Carlo model for gamma emissions, with an ICRU sphere irradiated from the surface. The beta doses to skin were calculated from published data for an epidermis equivalent depth in water corresponding to 0.4 mm thick clothing. In both cases, natural clearance from the skin, and radioactive decay of the isotopes, was taken into account. It was found that the largest dose contribution, both for gamma and beta emissions, came from I 134, with other significant doses arising from Cs 134 and Cs137. The gamma doses were found to be in the same range as those received over the first year following the Chernobyl accident from contamination of outdoor surfaces by dry deposition of aerosol.

In the remaining contractual period, efforts will continue to incorporate the experimental results in the model, and it is hoped that further experiments will determine whether it is appropriate to use a shorter clearance half-life than the COSYMA value (30 days) as model input. In addition, efforts will be made to increase the applicability of the model, which is currently linked to a case study in the Novozybkov area, and eliminate the uncertainties associated with the complex radionuclide dispersion process by expressing the calculated doses relative to an easily-measurable quantity: deposition on a grassed lawn.

To date, the model has calculated doses to a hairless person; future work will use the experimental data to estimate the effect of deposition and retention on hair in determining dose.

7 Annexes

7.1 Skin wiping protocol

Similar, but independent, protocols have been developed at Risø and at Imperial College. It should however be emphasised that this presents no disparity in the determination of deposition velocities. It is not the case that one protocol is better than the other ; provided that both are well validated, either is applicable. Furthermore, in understanding the basis of dermal exposure assessment techniques, the existence of two somewhat different protocols is useful.

Imperial College

1. Skin is exposed to tracer particles
2. In another area, wipe samples are prepared by an unexposed individual., from cotton fabric. The area of the individual wipes is approximately 10 cm². Wipes are soaked in distilled water
3. Exposed individual is removed from the test environment, and gloved.
4. A template is placed on the arm of the exposed person and held in place by the unexposed individual. The template is made of rigid steel, with a circular hole of diameter 4 cm (within which the skin is wiped).
5. The unexposed individual blots excess moisture from the wipe, and conveys it, via forceps, to the gloved hand of the exposed individual, who wipes his own arm.
6. The used wipe is transferred to a clean labelled plastic bag.
7. Steps 6 and 7 are repeated 5 times.
8. All wipes are analysed together in the same plastic bag.

Risø protocol

1. Skin is exposed to tracer particles.
2. In another area, the wipe samples prepared by an unexposed individual, from Whatman 542 filter paper. The area of the individual wipes is approximately 8 cm². The wipes are soaked in ethanol.
3. The exposed person is removed from the test environment
4. A template is placed on the arm of the exposed person and held in place by the unexposed individual. The template is made of flexible aluminium, with a rectangular hole of 8 cm², within which the skin is wiped. The unexposed individual blots excess moisture from wipe, and rigorously wipes the arm of the volunteer.
5. The used wipe is transferred to a clean labelled plastic bag.
6. Steps 4 and 5 are repeated 3 times.
7. All wipes are separately analysed

It has been found that despite differences in the sampling protocols, the removal efficiency of tracer is similar in both cases (quantitative wiping efficiencies were presented in the January 1997 report). Although cotton used at Imperial is more malleable than filter paper used at Risø as a wiping material, it is likely that ethanol, which may interact more effectively with grease on the skin than distilled water, may be a more effective “wetting agent”, so that the two techniques have comparable efficiency.

In both cases, measures were implemented which ensured that skin wiping was carried out in a rigorous and reproducible manner. At Risø, it was ensured that the same person always carried out the wiping, and this person was selected because he wiped in a particularly vigorous way. At Imperial College, it was feared that an element of restraint might be exercised in wiping the skin of another person, so that it was decided that the volunteers themselves would wipe their own skin. In the majority of cases (over 75%), the same volunteer was used.

7.2 The Imperial College Fluorescence Scanning System.

An alternative dermal exposure assessment technique to the use of neutron activatable aerosol tracers, and one which is completely non-invasive, is the use of aerosol labels in which fluorescence can be induced by appropriate illumination. The development of the Imperial College system for fluorescent labelling of aerosol particles and their subsequent illumination and detection, when deposited on skin, was preceded by a literature review of previous work, as summarised below. Fluorescence scanning has been used extensively as a non-invasive technique for investigating many types of surface contamination: in agriculture, the efficiency of pesticide spraying has been assessed by adding a fluorescent dye to the pesticide mix (Evans et al, 1992) and using an intensified machine vision system to characterise the pattern of spray deposits on leaves. With reference to semiconductor fabrication, Opiolka et al (1994) studied particle contamination of flat surfaces by using a microscope to detect the light emitted by polystyrene microspheres labelled with a fluorescent dye. Also, in the context of radioactive dose assessment following nuclear accidents, Cannell et al (1987) used a video camera with an image intensifier to detect the light emitted by fluorescent dye-labelled particles, and a microcomputer to analyse the signal, in their investigation of the mechanical transport of particulate con-

tamination into dwellings. Fluorescence scanning has been applied to the study of dermal contamination by several researchers. Fenske et al (1986), Bierman et al (1992), Archibald et al (1994) and Roff (1994) used ultra-violet fluorescence scanning systems, comprised of video cameras and microcomputers, to detect and quantify dermal exposure to chemicals such as pesticides. While most workers used plane banks of ultra- violet tubes to illuminate the subject and employed software algorithms to compensate for the curvature of the subject's surface, Roff (1994) used a dodecahedral arrangement of ultra-violet strip lights to provide uniform illumination of the subject's skin.

Most previous studies have addressed the issue of dermal contamination with fluorescent materials in highly-concentrated liquid forms; it was therefore possible to achieve strong fluorescent signals, so that interference from other sources, such as the skin itself, were not significant. The human skin is fluorescent under ultra-violet light (Anderson and Parrish 1982) and the level of skin auto-fluorescence may depend on the presence of dried skin or calluses (Vo-Dinh 1987) or the amount of previous exposure to sunlight. Since the anticipated fluorescence of tracer-labelled solid particles would be significantly less than that of liquids, the design of the Imperial College system included measures for avoidance of the interfering effects of skin auto-fluorescence. The main features of the Imperial College fluorescence scanning system are described below.

In a fluorescence scanning system, the tracer dye is induced to fluoresce by a excitation light source of a suitable wavelength. The emitted fluorescence is collected by a video camera and the analogue output is digitised by a frame grabber which is an input card connected to the computer. This input is a matrix of numbers which are proportional to the intensities of light collected by each pixel of the light-sensitive chip of the camera. Image processing software can then manipulate these numbers to deduce the quantity of tracer dye on the scanned surface. In order to minimise interference from skin auto-fluorescence, dyes that fluoresce strongly under visible light, rather than ultra-violet light, have been selected. The lighting used is high-power tungsten halogen white light, with the output filtered (by a Balzers Calflex 3000 heat mirror, combined with a Schott BG12 colour glass filter) to remove heat and give a monochromatic light at the excitation wavelength; the heat must be filtered out of the light output to give a constant operating temperature of 20 C for the excitation filter. The video camera purchased (Hitachi Denshi KPM1K monochrome) was chosen for maximum sensitivity to low light levels and has a filter (Schott OG515 colour glass filter) which blocks any reflected excitation light, thereby allowing only the fluorescent light into the camera. A fast computer (Dell Optiplex 560L), with a frame grabber (Matrox Comet), gives maximum speed of image processing. The image processing software used was Matrox Hi-Tools. The test aerosols used to date are monodisperse silica particles. The tracer dye, fluorescent isothiocyanate, may be attached to the silica particles by a method developed by Hodson et al (1994) to attach tracer dyes to plant silica fibres. The system described above has been tested for its ability to detect tracer-labelled particles, when deposited both on filter paper and on human skin. The tests indicate that the sensitivity of detection is significantly lower than neutron activation analysis, so that higher surface loadings of particles will be required for accurate quantitative analysis of fluorescent aerosol.

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Quantitative measurement of aerosol deposition on skin, hair and clothing for dosimetric assessment

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The deposition to human body surfaces of potentially hazardous aerosol has been investigated through tracer experiments. Particles of different sizes labelled with neutron activatable rare earth tracers were released in test rooms and deposited on volunteers. Various sampling techniques to examine the clearance and retention of the aerosol to skin, hair and clothing were investigated, and a protocol for the most efficient procedure was established and validated. Experiments indicate that the deposition velocity to skin increases linearly with the particle size. A wind tunnel experiment simulating outdoor conditions showed outdoor deposition velocities to be almost an order of magnitude higher than those recorded indoors. Both *in vivo* and *in vitro* experiments were conducted, and the influence of various factors, such as surface type, air flow, heating and electrostatics were examined. The dynamics of particle removal from human skin were studied by fluorescence scanning. Using the experimentally determined parameters, a model was established for calculation of radiation doses received from deposition of airborne radioactive aerosol on human body surfaces. It was found that the gamma doses that could be expected from deposition on skin were of the same order of magnitude as the gamma doses received over several years from contamination on outdoor surfaces. Assuming very high dry contamination levels, as were recorded in some areas of Russia after the Chernobyl accident, it was found that beta doses from skin deposition may amount to several Sievert and thus be responsible for a significant cancer risk.

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AEROSOLS; DEPOSITION; DYSPROSIUM 165; INDIUM 115; INDOOR AIR POLLUTION; PARTICLE SIZE; SAMPLING; SKIN; HAIR; CLOTHING; TRACER TECHNIQUES; CLEARANCE; FLUORESCENCE SCANNING; DOSES

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